

Son of NRPB-SR250



New Monte Carlo calculations at HPA-RPD for contemporary CT

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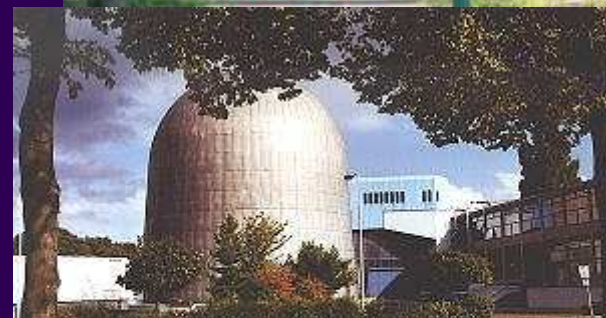
- History
- Changes
- New Monte Carlo calculations
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- Contemporary CT scanners
- Future

History – Where we are ... Who is Jan Jansen?



Expertise in Monte Carlo calculations with MCNP

- Dose conversion factors for: diagnostic radiology, screening mammography and CT
- Equivalent copper thickness of patient equivalent phantoms in terms of attenuation
- Determination of mean glandular tissue fraction
- Carcinogenic risk of radiotherapy for benign diseases



History – Where we are ... NRPB Reports



NRPB-R249

NRPB-SR250 (1993)

Survey of CT Practice in the UK

Part 2: Dosimetric Aspects

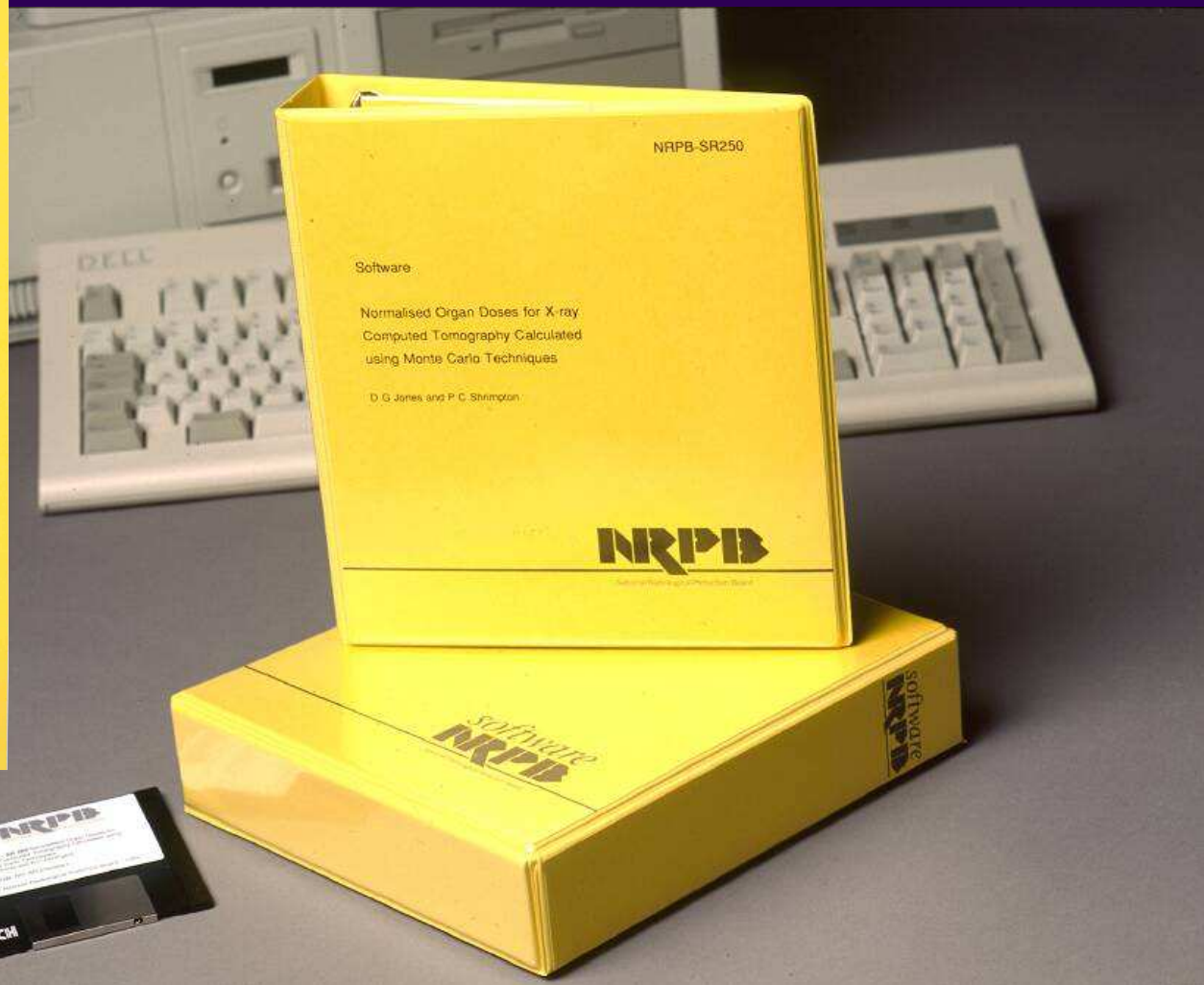
P C Shrimpton, D G Jones, M C Hillier,
B F Wall, J C Le Heron and K Faulkner

NRPB-R249



National Radiological Protection Board

NRPB- R248-250 (1991)



History – Where we are ...

NRPB-SR250



NRPB-SR250 (1993)

- 23 series of Monte Carlo calculations for 27 scanner models
- 208 sets (5 mm slabs) of normalised dose data for ...
- 27 organs or regions of a mathematical phantom

More user-friendly access of data files

- Program to read the data files by J.C. Le Heron. CTDOSE: a user's guide. Software and manual. (National Radiation Laboratory, New Zealand (1993) (No longer available)
- ImPACT CT Patient Dosimetry Calculator Spreadsheet (2000-2006)
 - Matches scanners to the 23 Monte Carlo calculations

History – Where we are ... After NRPB-SR250



Work at the NRPB after SR250 by Amjad Khursheed

- Change of hardware from DEC-VAX to PC
- Change in operating system from VMS to MS-DOS / MS Windows (command-line window)
- Change in Monte Carlo code from home-made to MCNP4C
- Change in anthropomorphic phantoms from home-made MIRD compatible hermaphrodite adult to MCNP input based MIRD compatible hermaphrodite adult and newborn, 1, 5, 10 and 15 year olds
- Three scanners: GE 9800, Siemens Somatom DRH and Philips LX.

Changes – Why the Need?



Scanner

- Multi-slice scanners
- Spiral
- Tube current modulation or Automatic Exposure Control
- X-ray tube, computer speed and rotation time development

Patient model

- Voxel instead of mathematical phantoms
- Bone dosimetry
- Draft ICRP recommendations

Changes – Why the Need?



Monte Carlo calculation

- Software development from home-made to general codes
- Hardware from Workstation to PC Cluster

Dosimetry

- Increasing CT doses reported
- Paediatric CT examinations are increasing

Monte Carlo Calculations - Set-up

Computer Cluster

- 7 nodes each with
 - 2x Dual Core AMD Opteron processors
 - 8 GB of memory
- Ethernet switch
- KVM switch

Software

- Linux Fedora Core
- MCNPX and MCNP5 (LANL)
- Intel Fortran 95 compiler
- OpenPBS



Quality Assurance – Comparing SR250 & MCNPX Results



Three scanners

- General Electric 9800
- Siemens DRH
- Philips LX

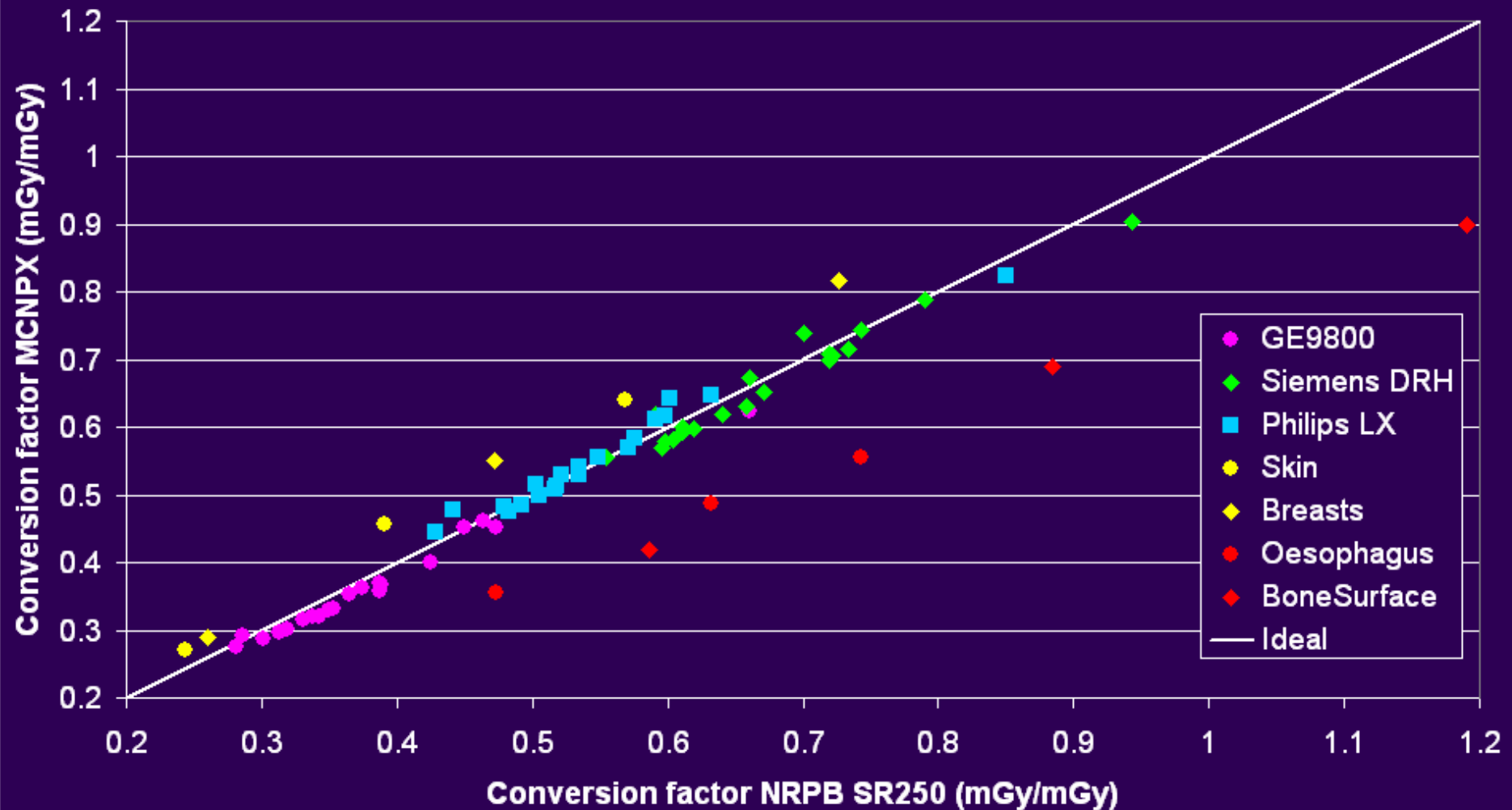
Comparison of the three scanners

- High consistency between old and new calculations
 - Normalised organ doses ($D_{\text{Organ}} / \text{CTDI}_{\text{Free-in-air}}$) for various organs
 - Highlighting organs with more than 10% difference
 - Highlighting organs with more than 30% difference

Quality Assurance – Comparing SR250 & MCNPX Results



Organ dose per CTDI (mGy/mGy) for MCNPX versus NRPB SR250



Quality Assurance – Comparing SR250 & MCNPX Results



Comparing various calculation techniques for the Philips LX Table with ratios of normalised organ doses for all slices for various different calculation methods

| Source | Rotation | Bone Dose | Min | Max | $E_{ICRP-60}$ |
|--------|------------|-----------|--------------------|------|---------------|
| Line | Continuous | ORNL | 1 | 1 | 1 |
| Line | Continuous | NRPB | 0.43 BS 0.90 BM | 1 | 0.97 |
| Line | Discrete | ORNL | 0.98 | 1.03 | 1.00 |
| Point | Continuous | ORNL | 1.02 | 1.05 | 1.03 |

Contemporary CT scanners – Example of the work



Information needed from CT manufacturers

Hardware

- Geometry
- Bow-tie filter, position, shape and material
- X-ray source description in tube voltage, filtration (thickness and material) and anode angle

Software (means of operation)

- Automatic exposure control
- Tube current modulation (minimum and maximum tube current)
- How to get user access to the tube current data?

Contemporary CT scanners – Example of the work



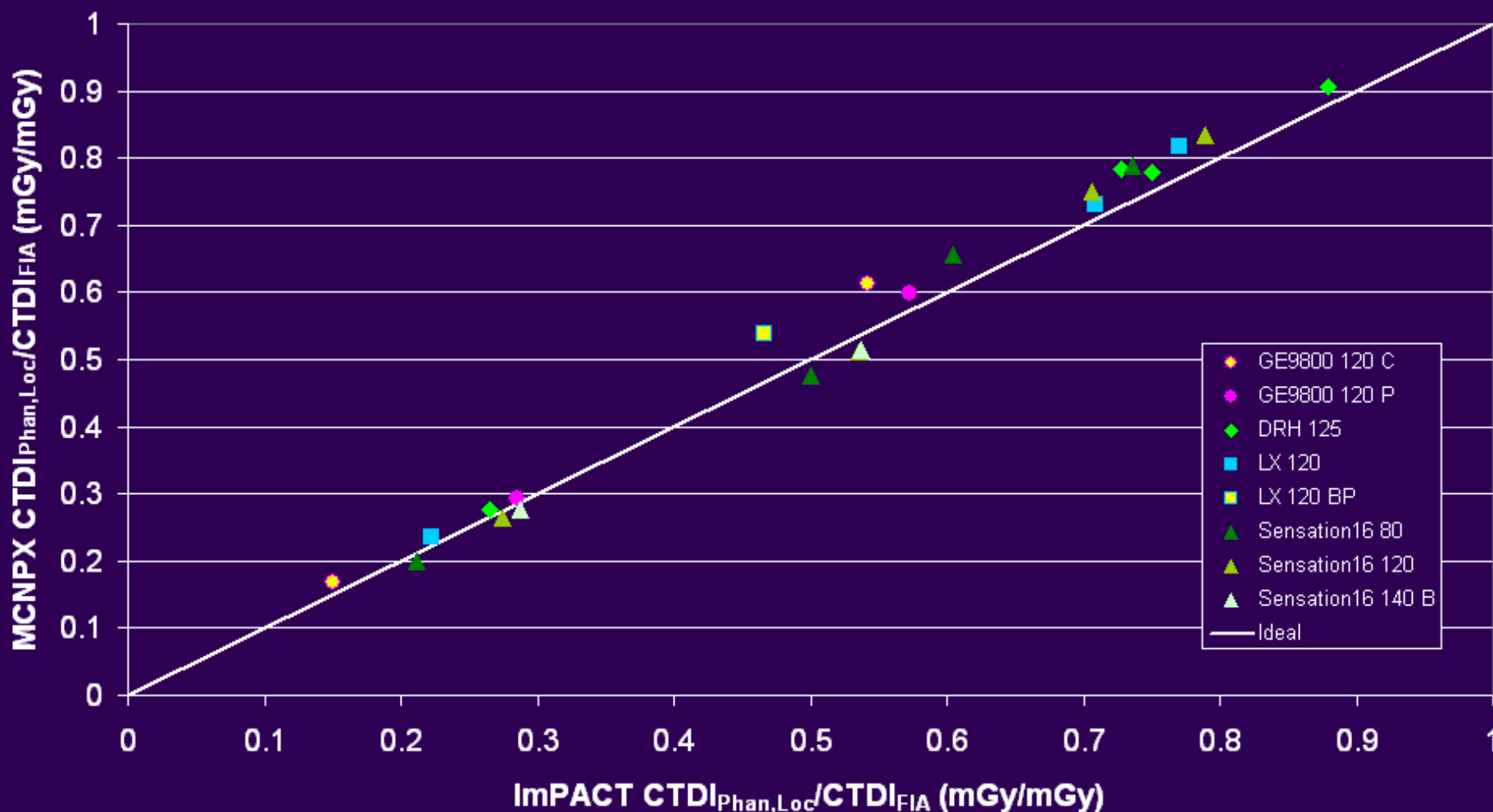
As an example, the Siemens Somatom Sensation 16

- Tube voltage: 80, 100, 120 and 140 kV
- Filtration: 3 mm Al + 1.2 mm Ti + 1.6 mm PTFE (Body)
3 mm Al + 0.6 mm Ti + 1.6 mm PTFE (Head)
- Tube current: constant, AEC (function of z derived from topogram), tube current modulation (function of angle derived from previous half scan) and AEC and tube current modulation
- Collimation (mm): 1.2, 2, 9, 10, 12, 18 and 24 mm
- Pitch
- Scan area on the patient

Contemporary CT scanners – CTDI Phantom



CTDI_{phan,loc} per CTDI_{FIA} for MCNPX versus ImPACT



Contemporary CT scanners – Siemens Sensation 16



Effective dose per CTDI_{FIA} calculated with MCNPX & ImPACT

| Tube voltage (kV) | Examination | E/CTDI _{FIA} MCNPX (mSv/mGy) | ICRP-60 +RR +MWR -MWC Match ImPACT (mSv/mGy) | Organ |
|-------------------|-------------|---------------------------------------|--|---------|
| 80 | Head | 0.020 | 0.021 | Brain |
| 120 | Head | 0.027 | 0.022 | Brain |
| 80 | Chest | 0.15 | 0.17 | Thymus |
| 120 | Chest | 0.19 | 0.19 | Thymus |
| 140 | Chest | 0.20 | 0.23 | Thymus |
| 80 | Abdomen | 0.12 | 0.12 | Kidneys |
| 120 | Abdomen | 0.15 | 0.14 | Kidneys |
| 140 | Abdomen | 0.16 | 0.17 | Kidneys |
| 80 | Pelvis | 0.13 | 0.14 | |
| 120 | Pelvis | 0.17 | 0.17 | |
| 140 | Pelvis | 0.18 | 0.19 | |

Contemporary CT scanners – Sensation 16, 120 kV



Effective dose per $CTDI_{FIA}$ calculated with Remainder Rule and +/- Mass Weighed Remainder and Colon, and using new ICRP Draft

| Examination Program | Effective dose / $CTDI_{FIA}$ (mSv/mGy) | | | | |
|---------------------|---|---|---|---|--------|
| MWR | - | + | + | + | Draft† |
| MWC | - | - | - | + | |

| | | | | | |
|---------|-------|-------|-------|-------|-------|
| Head | MCNPX | 0.027 | 0.027 | 0.027 | 0.034 |
| Head | SR250 | 0.022 | 0.022 | 0.022 | 0.028 |
| Chest | MCNPX | 0.19 | 0.19 | 0.19 | 0.21 |
| Chest | SR250 | 0.18 | 0.18 | 0.18 | 0.21 |
| Abdomen | MCNPX | 0.15 | 0.15 | 0.17 | 0.15 |
| Abdomen | SR250 | 0.15 | 0.14 | 0.16 | 0.15 |
| Pelvis | MCNPX | 0.17 | 0.17 | 0.16 | 0.14 |
| Pelvis | SR250 | 0.17 | 0.17 | 0.15 | 0.13 |

† With surrogate organs

Future – Where we go



Available in the near future

- ICRP standard anthropomorphic voxel phantoms
- Draft ICRP recommendations for effective dose
- Manufacturer CT scanner information

Needed but probably not available until the distant (?) future

- User access to tube current data

Conclusions - Summary



- The PC cluster is ready to perform calculations!
- Preparation of new conversion factors is timely
- Organ dose conversion factors from MCNPX are within 10% of SR250 values (with known exceptions for 4 organs)
- Differences in source simulation (parallel line vs divergent point, and continuous vs discrete) are small (<5%)
- Changes in bone dosimetry from NRPB to ORNL could increase the red bone marrow dose by 10% and the bone surface dose by a factor of 2.3
- ImPACT match for Sensation 16 is a good approximation for E (ICRP 60) in sample examinations (mostly <10%)
- Draft ICRP recommendations (implemented with surrogate organs) result in larger differences in E (up to 30%)