

# Comparison of the function and performance of CT AEC systems



*CTUG meeting*

by

Emily Field

Trainee clinical scientist

# Breakdown

- CT Automatic Exposure Control (AEC)  
Background
- Project Description
  - Aim
  - Methodology
  - Results
  - Conclusion

# AEC systems in CT

## *What is the aim of AEC in CT?*

- To minimise or remove variations in image quality between different images.
- To reduce variation in doses delivered to patients of varying sizes/shapes.

## *How is this achieved?*

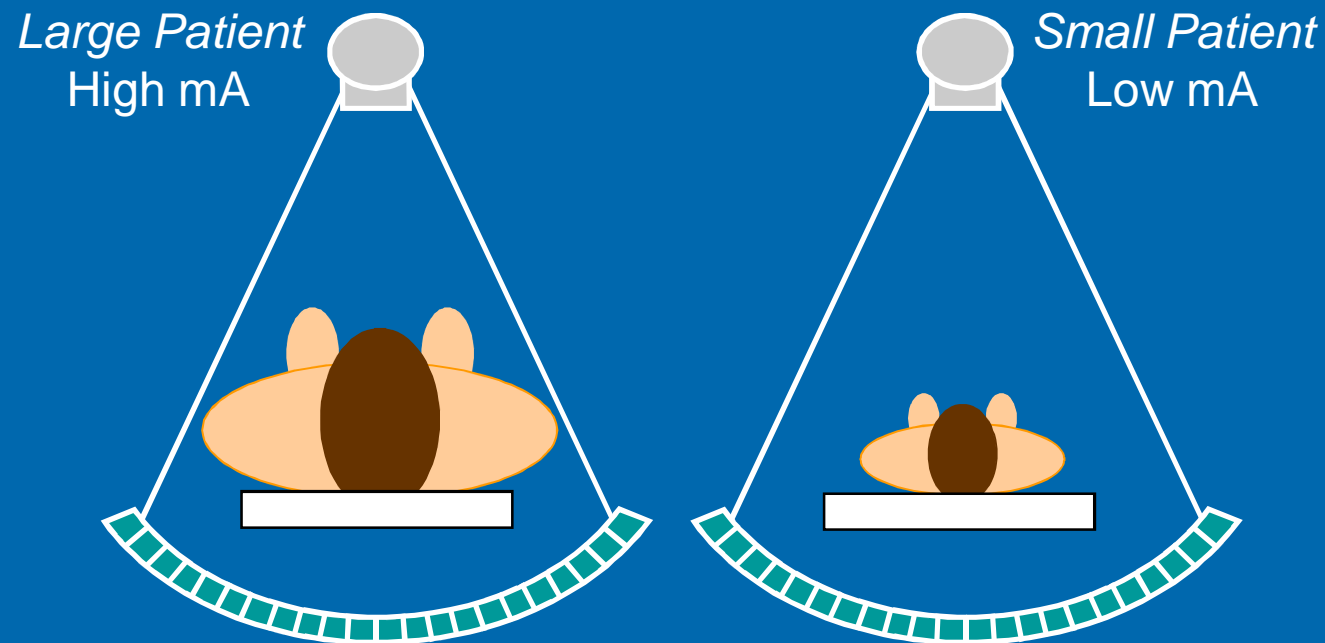
- This is made possible in CT scanning by controlling the **tube current (mA)** during scanning to achieve the required level of image noise. This is also known as *mA modulation*.

Modern CT scanners can achieve mA modulation in 3 distinct ways.....

# AEC systems in CT

## 1. Patient size AEC

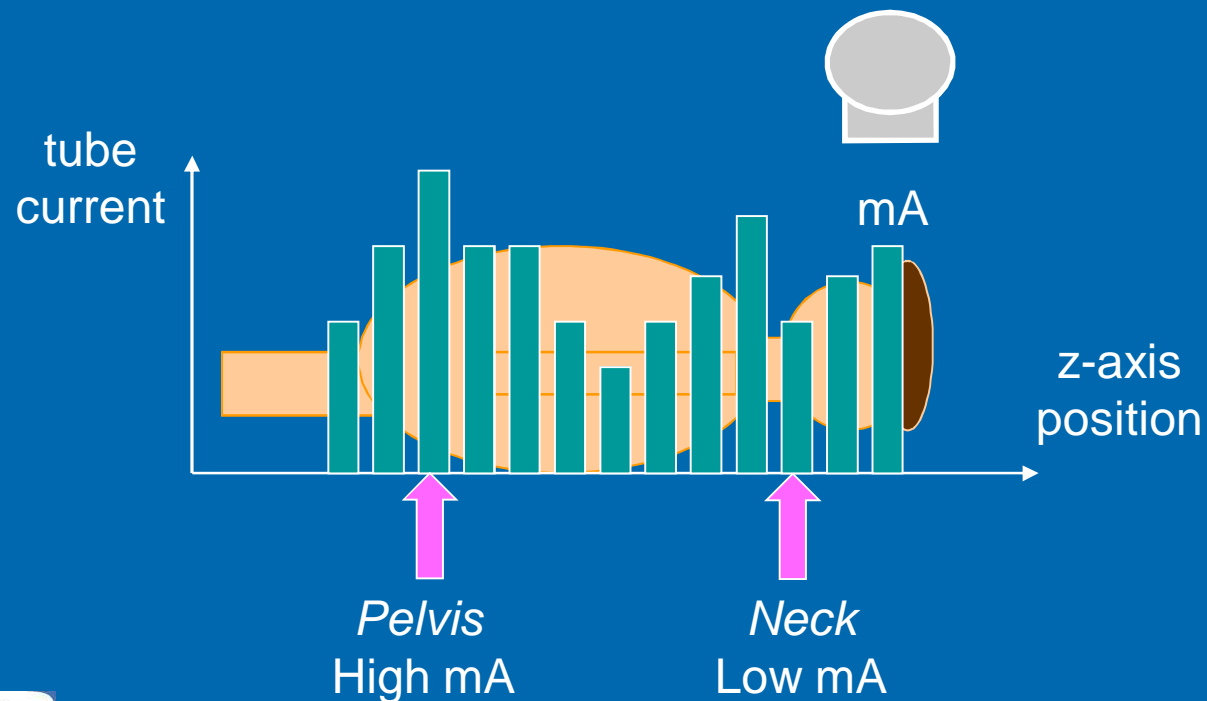
- mA is adjusted grossly based upon the overall size of the patient.



# AEC systems in CT

## 2. Z-axis AEC

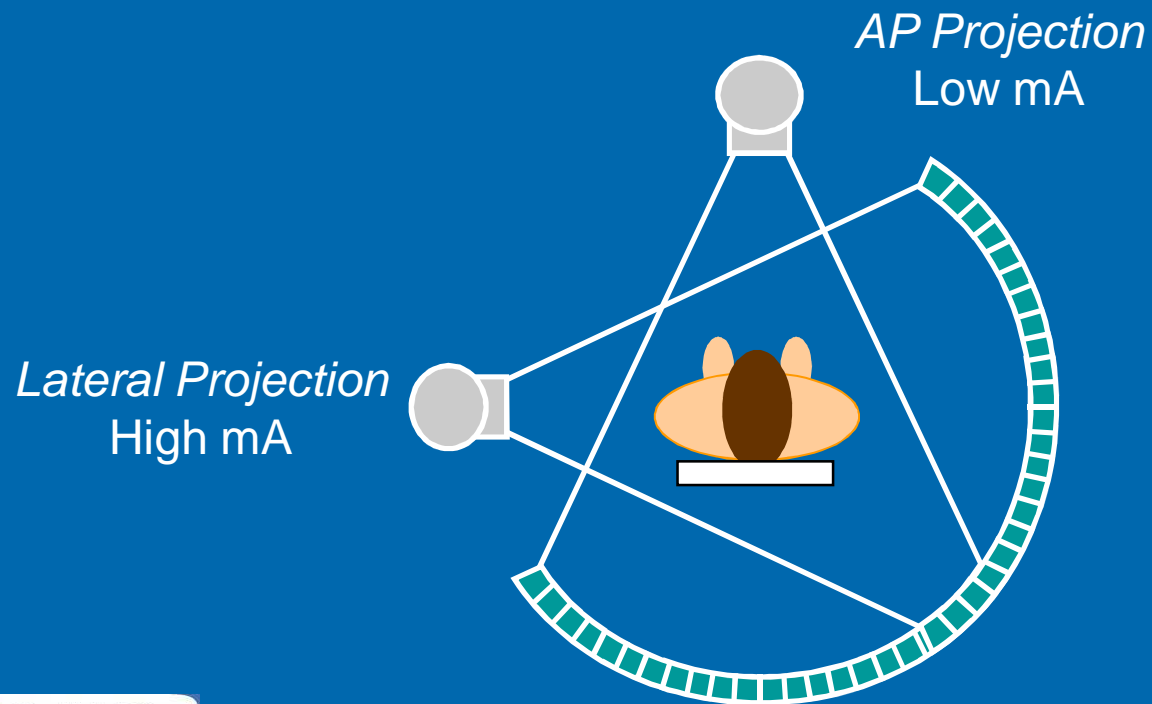
- Variations in attenuation along the length of the patient are compensated for by adjusting the mA for each successive tube rotation.



# AEC systems in CT

## 3. Rotational AEC

- mA is adjusted during a single rotation of the tube to compensate for differences in attenuation between AP and Lateral projections.

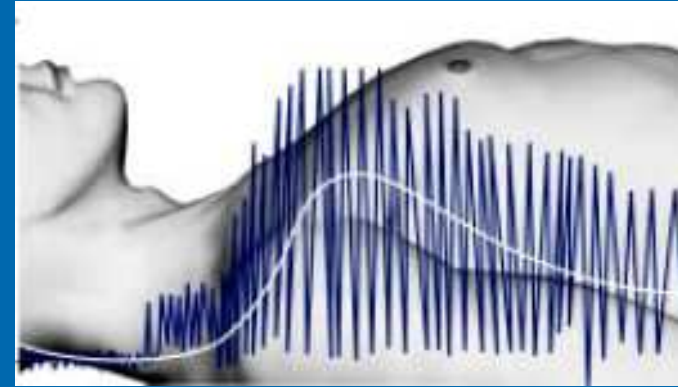


# AEC systems in CT

- In reality, **all three** AEC systems operate simultaneously.

## ***Patient and z-axis AEC***

- The main source of patient attenuation data necessary for operation of the AEC system is acquired during the *scan projection radiographs (SPRs)*. These are also known as scouts, topograms or scanograms.



## ***Rotational (x, y – axis) AEC***

- Feedback - changes in patient profile occur gradually along the z-axis, many systems utilise real-time feedback to inform the system of the changes in attenuation. For example, the patient attenuation data acquired during a single rotation can be used to inform the system of the optimum mA settings for the subsequent rotation.
- SPR - asymmetry of the patient can be estimated from SPRs and the x-ray tube current varied accordingly.

# AEC systems in CT - Benefits

## *What are the overall benefits?*

- **Consistent image quality** - User defined levels of image noise achievable from slice to slice but also from patient to patient.
- **Potential to reduce patient exposure** - A fully optimised CT system can avoid unnecessary exposure of the patient.
- **Reduced tube loading** - Modulated mA runs have the potential to reduce the overall loading of the x-ray tube.
- **Extended scan runs** - A reduction in x-ray tube heating means that longer scan runs can be utilised where necessary.
- **Reduction of photon starvation artefacts** - Rotational AEC means that previously under-sampled lateral projections (e.g. across shoulders) can be avoided.



# AEC systems in CT

- Each major CT manufacturer has their own version of AEC.

Manufacturer	Patient size AEC	Z-axis AEC	Rotational AEC	Method for setting exposure level
<i>GE</i>	AutomA	AutomA	SmartmA	“Noise Index”
<i>Siemens</i>	Care Dose 4D	Care Dose 4D	Care Dose 4D	“Reference mAs”
<i>Toshiba</i>	Sure Exposure	Sure Exposure	Sure Exposure 3D	Standard deviation
<i>Philips</i>	DoseRight ACS	-	DoseRight DOM	“Reference image” noise level

# Study Aim

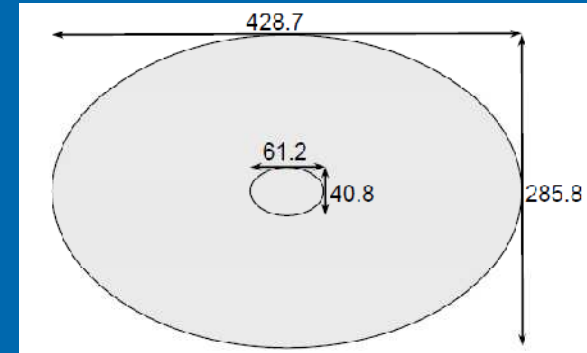
*To assess the efficacy of a range of CT scanner AEC systems using a homogeneous elliptical cone phantom. Variations in performance characteristics between scanner models and manufacturers was also investigated.*

# Scanners Tested

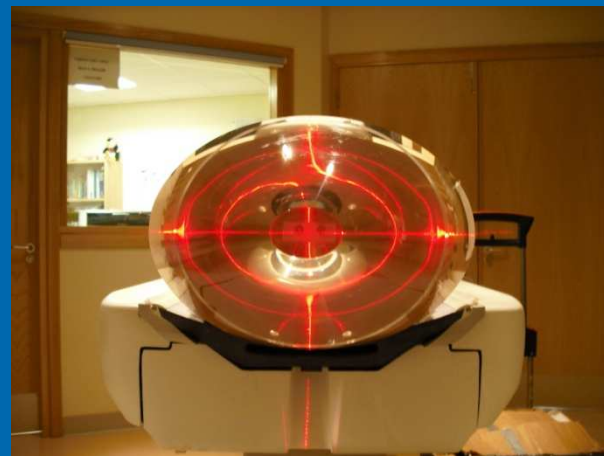
Hospital Site	Scanner	Make/Model	Slice
<i>A</i>	CT1	Toshiba Aquilion	64
	CT2	Toshiba Aquilion	16
<i>B</i>	CT	Toshiba Aquilion	64
<i>C</i>	CT	Toshiba Aquilion	64
<i>D</i>	CT	Toshiba Aquilion	64
<i>E</i>	CT1	GE Discovery HD750 (dual kV) with ASIR	64
	CT2	GE Lightspeed	16
	CT3	GE Lightspeed	64
<i>F</i>	CT	GE Lightspeed with (ASIR)	8
<i>G</i>	CT	GE Lightspeed	64
<i>H</i>	CT	Siemens Sensation	64

# Methodology – The Phantom

- Homogeneous, acrylic, elliptical, cone-shaped phantom.
- Same phantom used by ImPACT for their 2005 report<sup>1</sup> (Thank you!).
- Designed to test each distinct AEC system (z-axis, rotational etc...)



Phantom dimensions (30cm z-axis length).



<sup>1</sup> CT scanner automatic exposure control systems. Medicines and Healthcare Regulatory Agency, February 2005. Report 05016

# Methodology – Standard Settings

- Standardised test protocol for every CT scanner attempted for fair comparison (*120kVp, 1sec rot time, standard reconstruction parameters, 5mm slice recon, large FOV*).
- However, slight variations unavoidable between models/manufacturers (below).

Manufacturer	Detector Rows	Collimation (mm)	Helical /Axial	Pitch	AEC system	Image quality settings
<i>GE</i>	64	2x5	Axial	-	AutomA, SmartmA	NI 10, 10-750mA
	16	8x1.25	Axial	-	AutomA, SmartmA	NI 10, 10-750mA
	8	8x1.25	Axial	-	Auto mA	NI 10, 10-440mA
<i>Siemens</i>	64	64x0.6	Helical	0.6	CARE Dose 4D	Average, 210 quality ref
<i>Toshiba</i>	64	16x0.5	Helical	0.938	SureExposure4D	SD 10, 10-380mA
	16	16x0.5	Helical	0.938	SureExposure4D	SD 7.5, 80-410mA

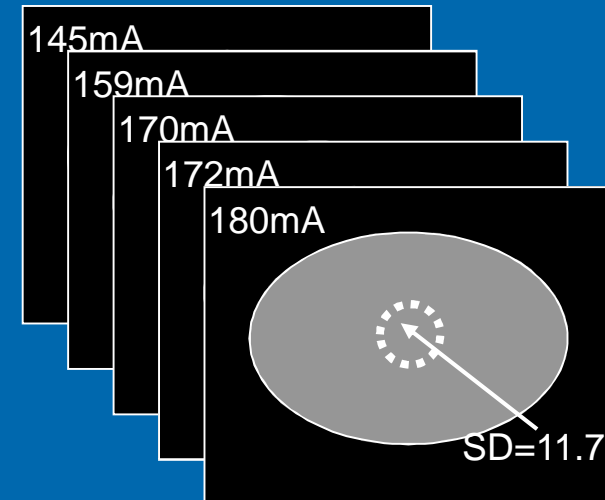
# Methodology

- Scan projection radiographs (SPRs) acquired (AP and lateral) along entire phantom length.
- Scans of complete phantom length planned and performed from SPR images (based on previously described standard settings).
- Resulting sequence of images analysed in terms of two key parameters;

1. Delivered mA for each slice (related to absorbed dose)
2. Standard deviation of CT numbers in central ROI (measure of noise)

- The effect of adjusting several parameters on applied x-ray tube current and image standard deviation (noise level) were recorded;

- kV
- Pitch
- Reconstruction kernel
- AEC image quality setting e.g. noise index



# Results

The following results are for 64-slice  
scanners only

# AEC on/off



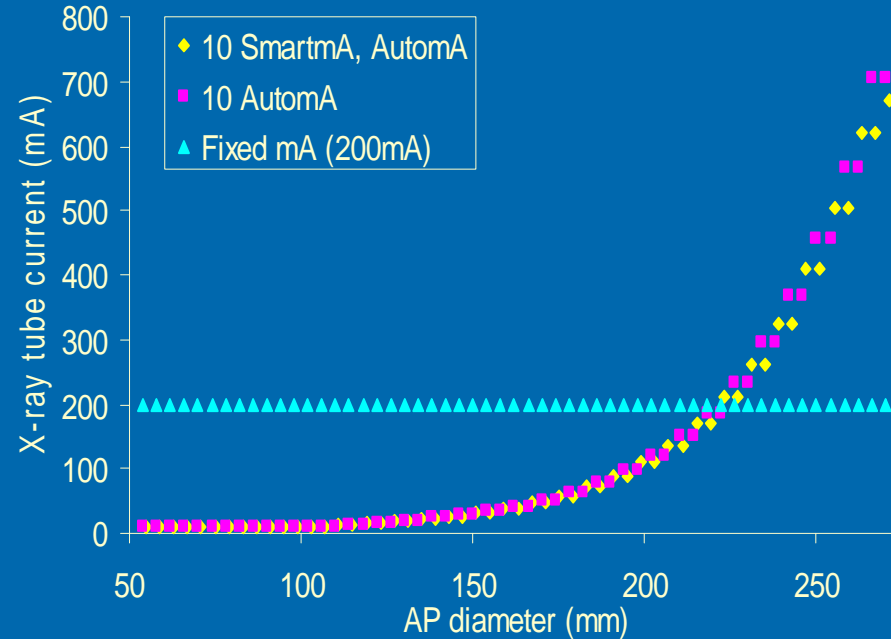
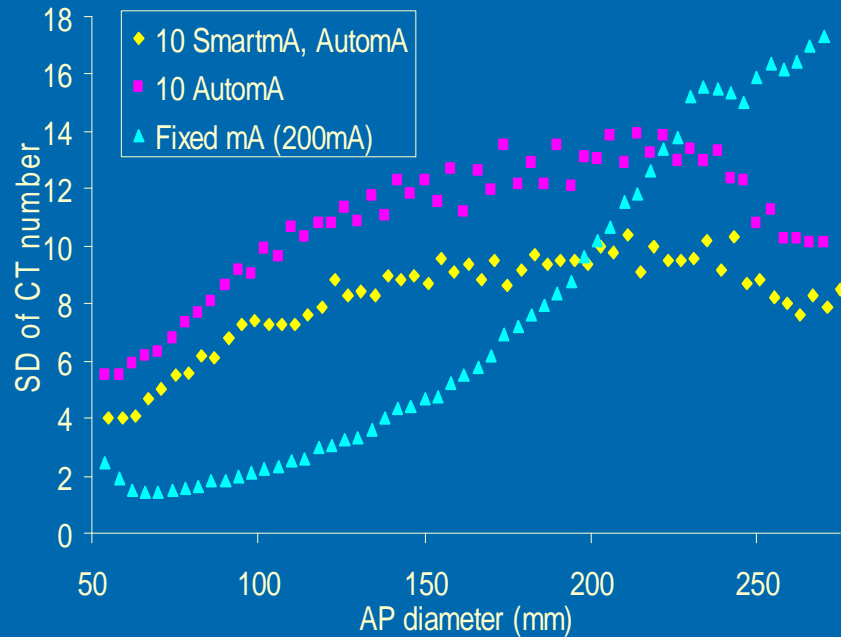
GIG  
CYMRU  
NHS  
WALES

Bwrdd Iechyd Prifysgol  
Caerdydd a'r Fro  
Cardiff and Vale  
University Health Board

14<sup>th</sup> October 2010

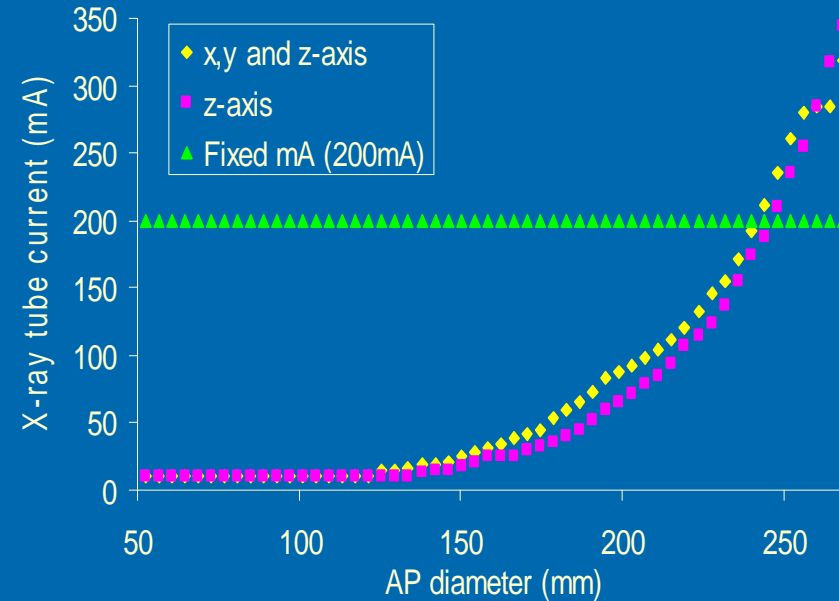
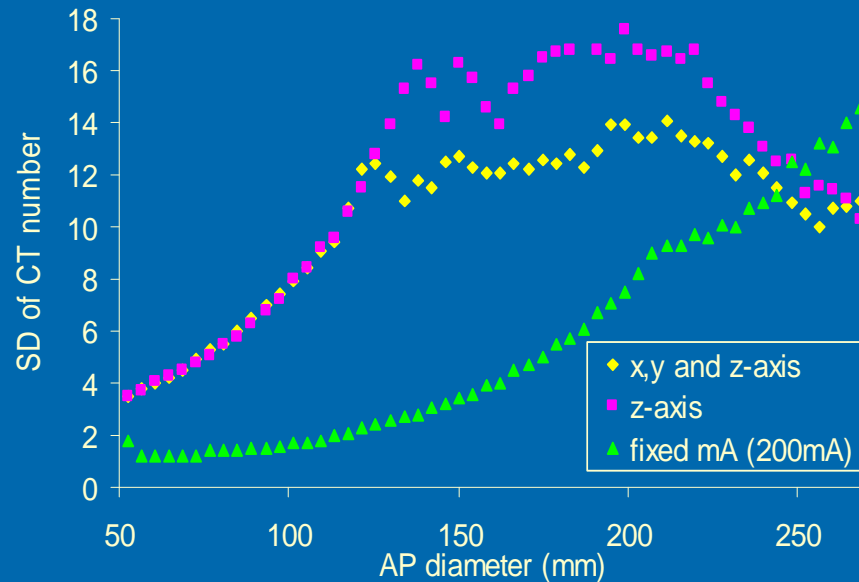


# Results - GE



- AEC system maintains image quality as the AP diameter is increased.
- Image quality is improved when AutomA is combined with SmartmA

# Results - Toshiba



- AEC system maintains image quality as the AP diameter is increased.
- Image quality is improved when z-axis AEC is combined with x, y-axis AEC.

# Results - Siemens

- Siemens z-axis and x, y-axis AEC system CareDose4D could not be operated independently.
- CareDose4D could either be selected with both AEC systems working together or not at all.

# Varying image quality

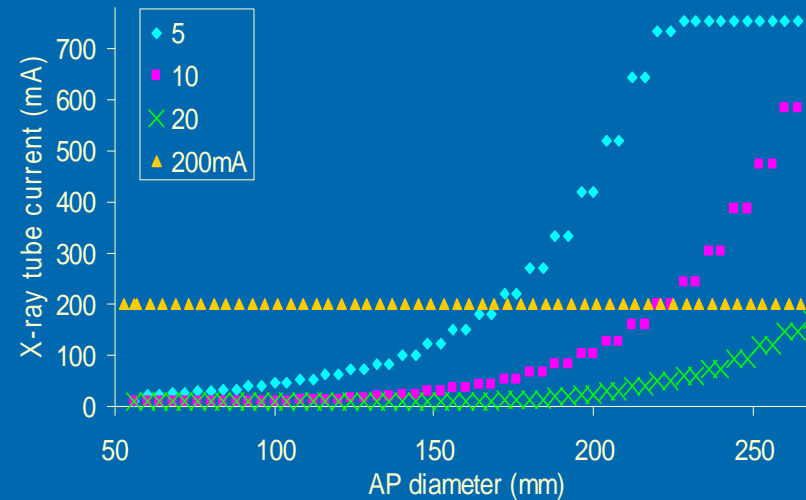
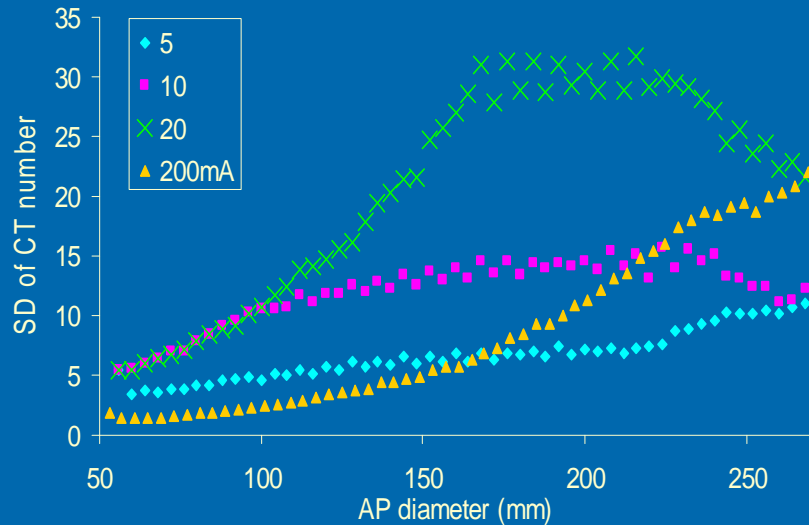


GIG  
CYMRU  
NHS  
WALES

Bwrdd Iechyd Prifysgol  
Caerdydd a'r Fro  
Cardiff and Vale  
University Health Board

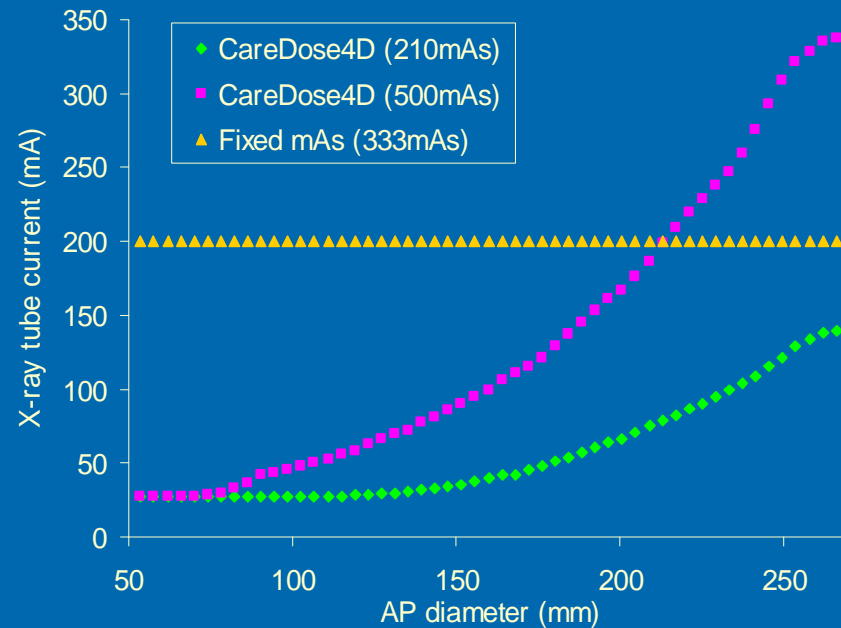
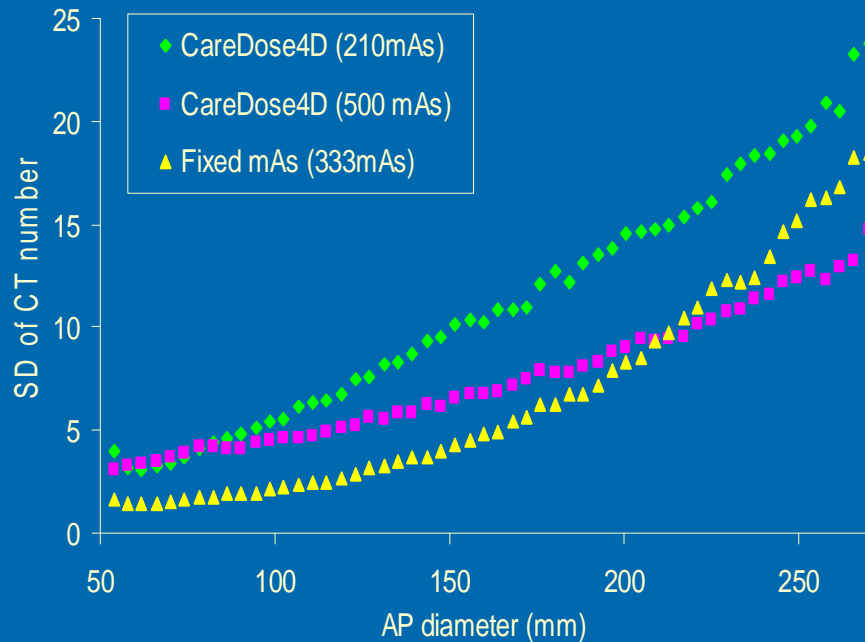
14<sup>th</sup> October 2010

# Results - GE



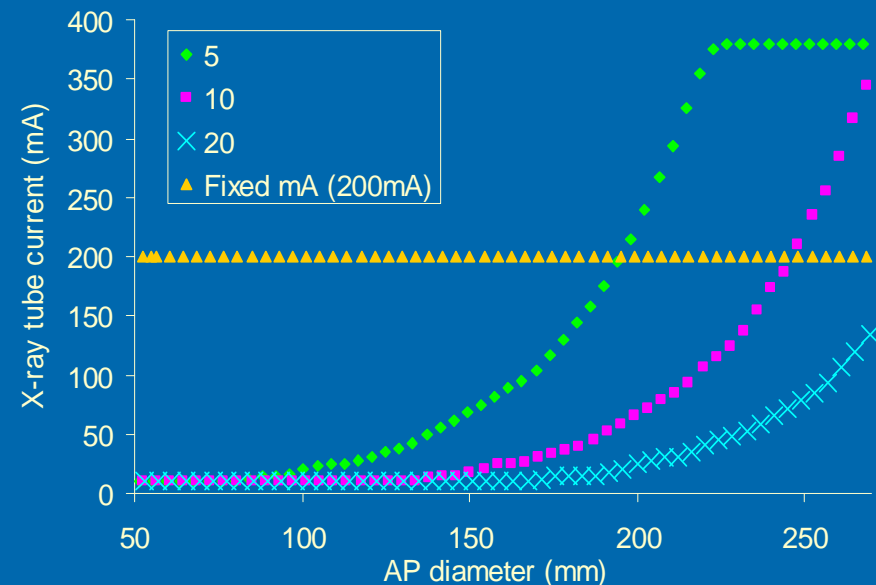
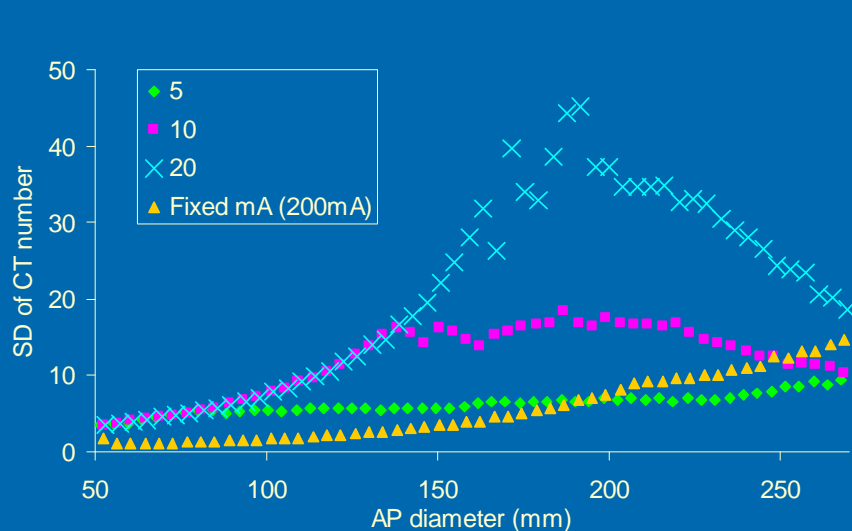
- Increasing image quality increases mA.
- Image quality is maintained at the required level more accurately at lower NI values.

# Results - Siemens



- Increasing the quality reference mAs increases the mA modulation.
- Image noise reduced for smaller AP diameters than larger ones. Therefore reducing the image noise for smaller patients and increasing it for larger ones (where it is more tolerable).

# Results - Toshiba



- AEC system behaves in a similar fashion to GE
- Increasing image quality increases mA.
- Image quality is maintained at the required level more accurately at lower SD values.
- Increasing SD increases the AP diameter at which mA begins to be modulated.

# Varying tube voltage



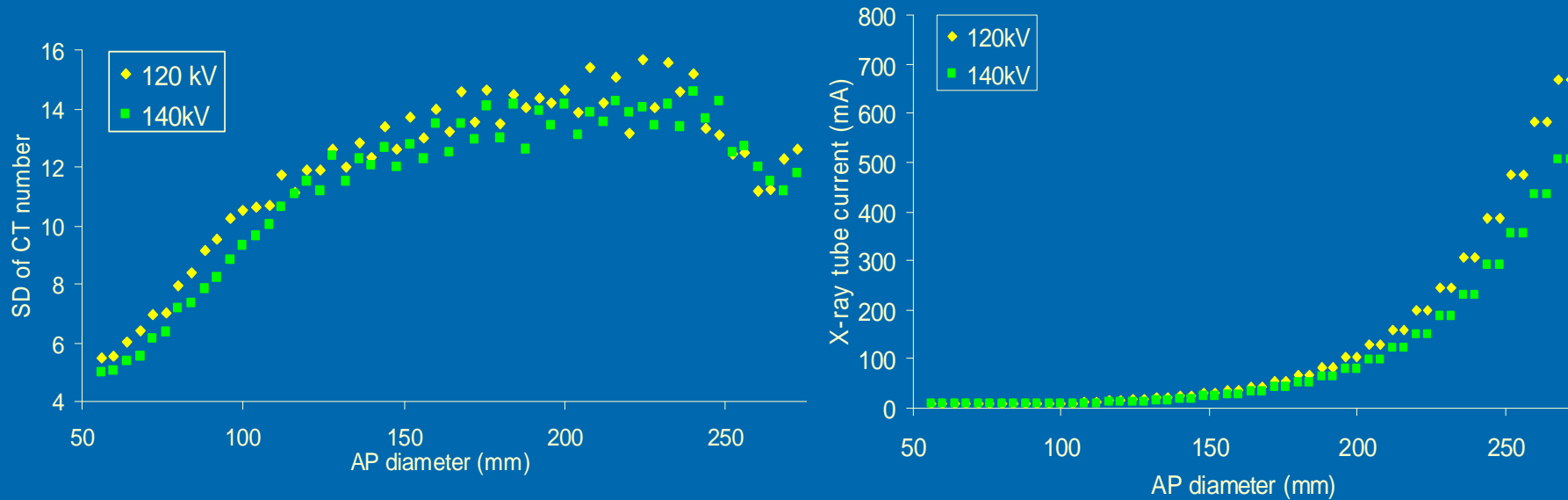
GIG  
CYMRU  
NHS  
WALES

Bwrdd Iechyd Prifysgol  
Caerdydd a'r Fro  
Cardiff and Vale  
University Health Board

14<sup>th</sup> October 2010

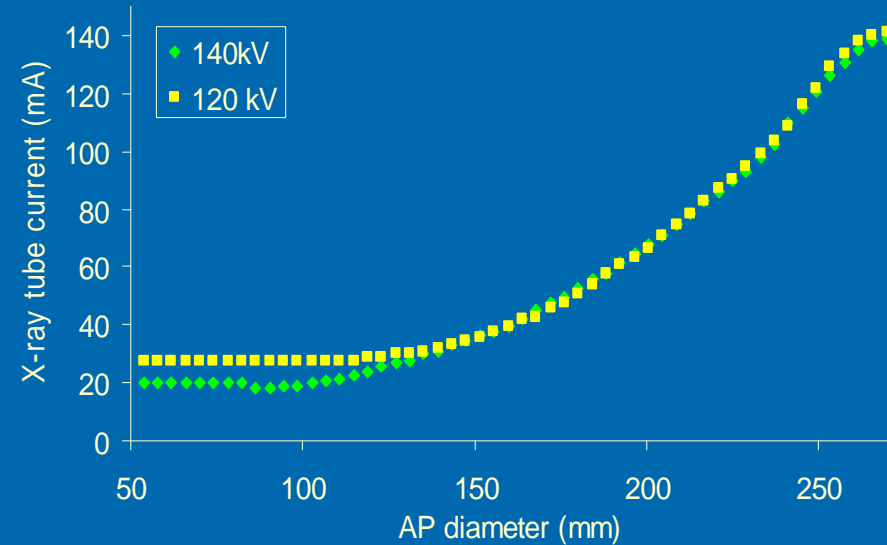
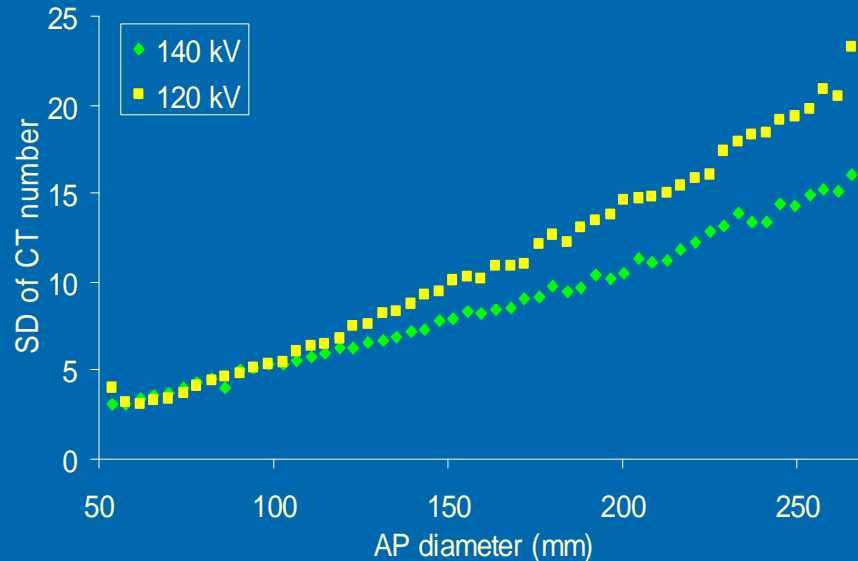


# Results - GE



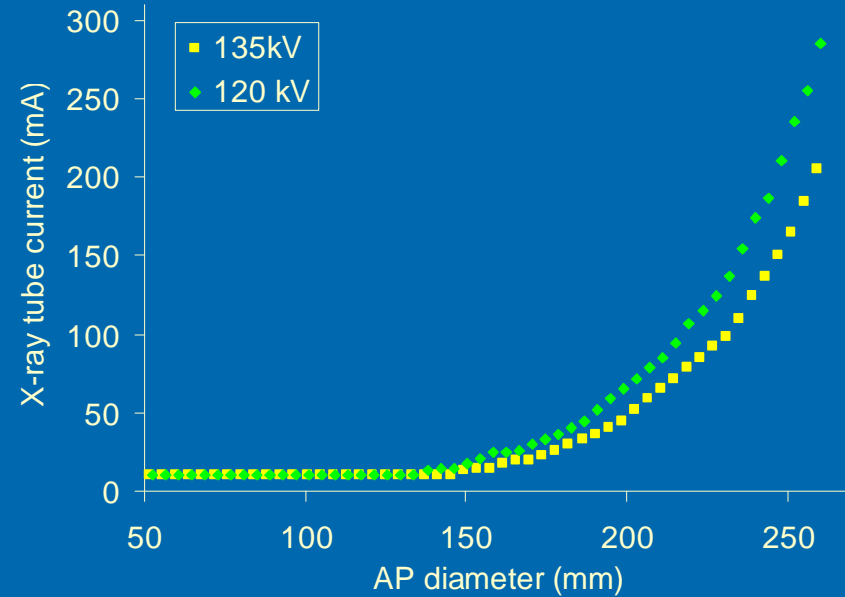
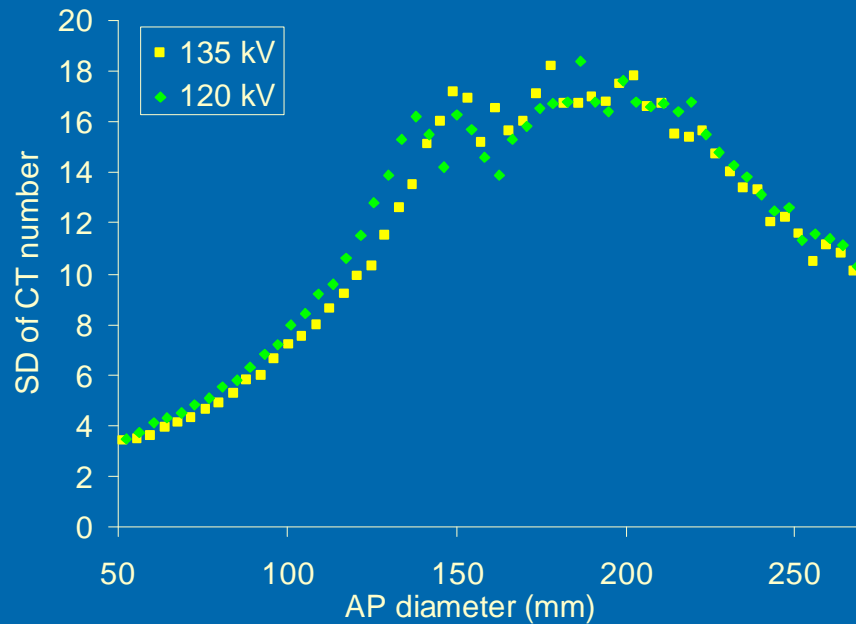
- Changing kV does not alter image quality.
- mA decreases when kV increases to maintain image quality.

# Results - Siemens



- Increasing kV increases the image quality, whilst mA remains constant at AP diameters greater than 130mm.

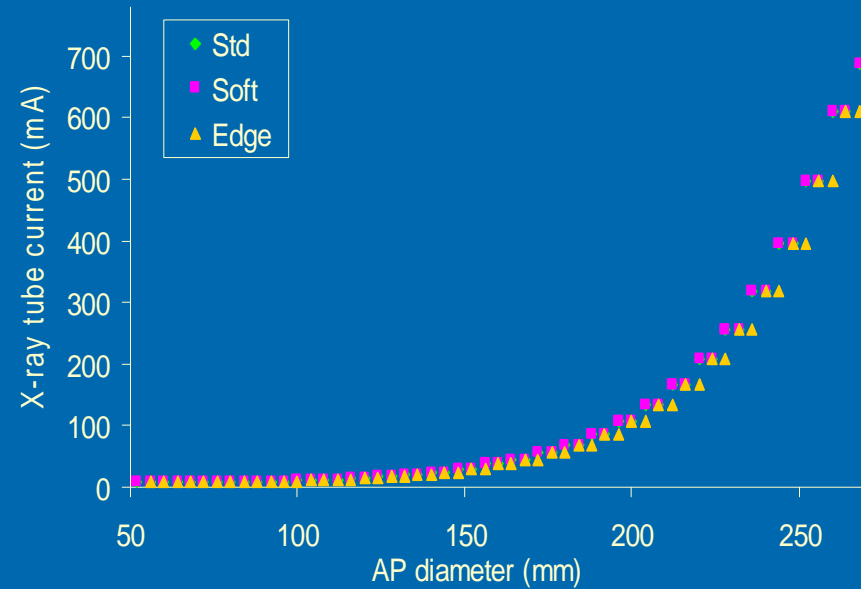
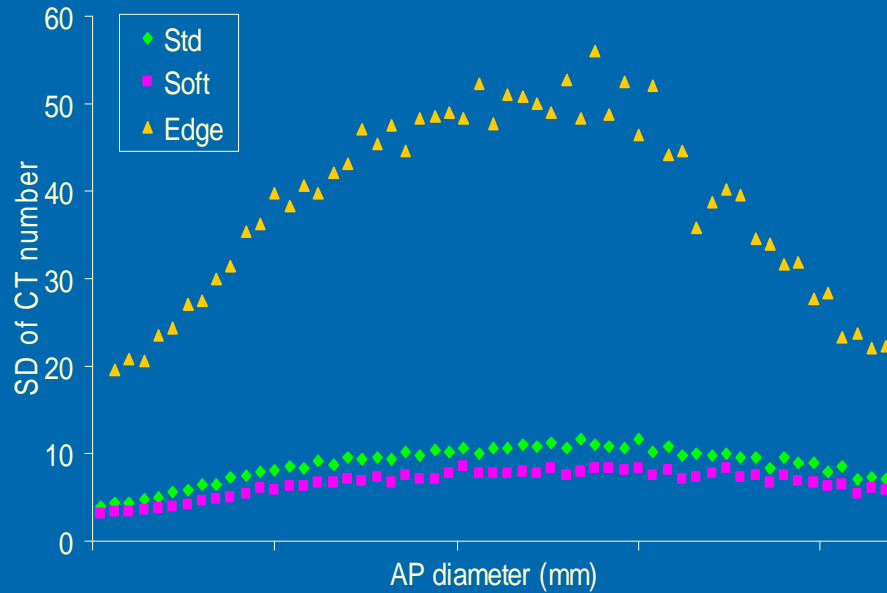
# Results - Toshiba



- Changing kV does not alter image quality.
- mA decreases when kV increases to maintain image quality.

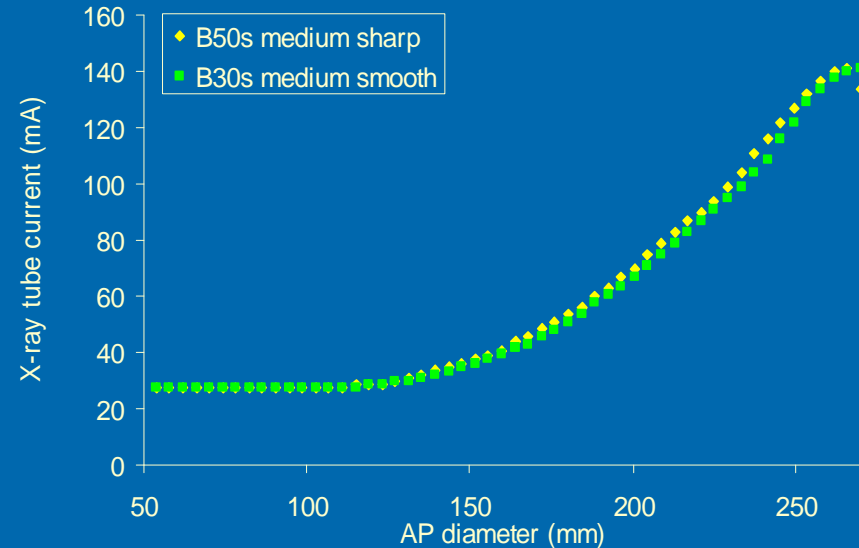
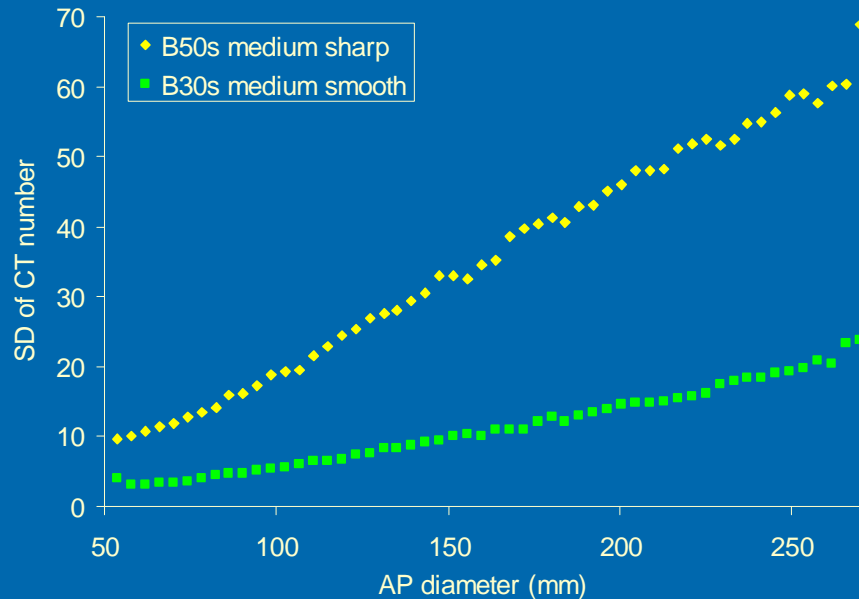
# Varying reconstruction kernel

# Results - GE



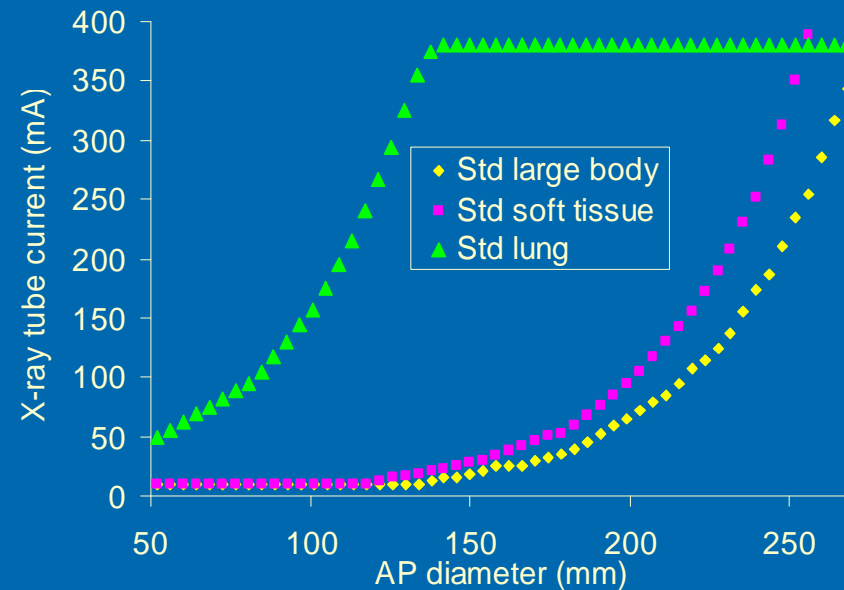
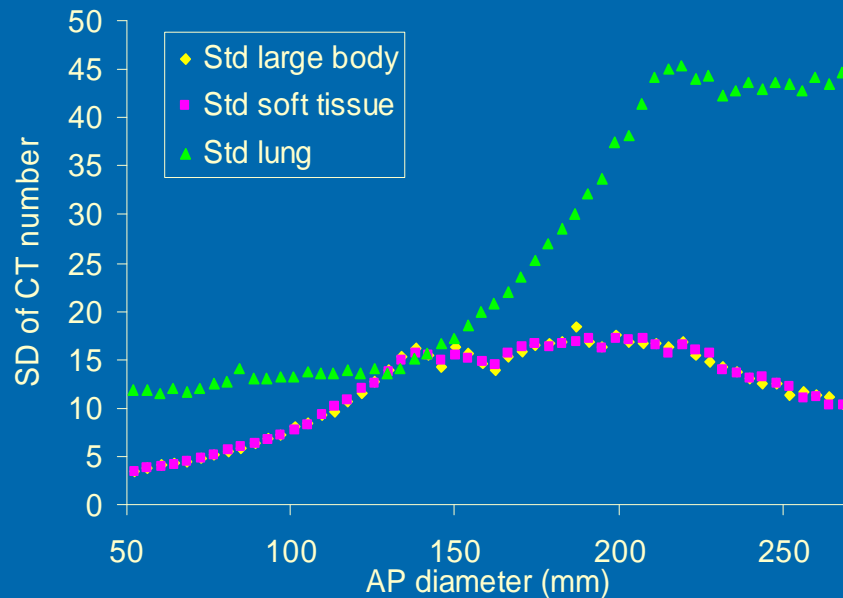
- Changing the reconstruction algorithm changes the variation in CT number for each pixel making up the image to alter the appearance.
- Reconstruction algorithm chosen did not alter the mA applied.

# Results - Siemens



- Behaves similar to GE.
- Changing the reconstruction algorithm changes the variation in CT number for each pixel making up the image to alter the appearance.
- Reconstruction algorithm chosen did not alter the mA applied.

# Results - Toshiba



- Changing the reconstruction algorithm changes the variation in CT number for each pixel making up the image to alter the appearance.
- Reconstruction algorithm chosen alters the mA applied along the phantom length.

# Varying pitch



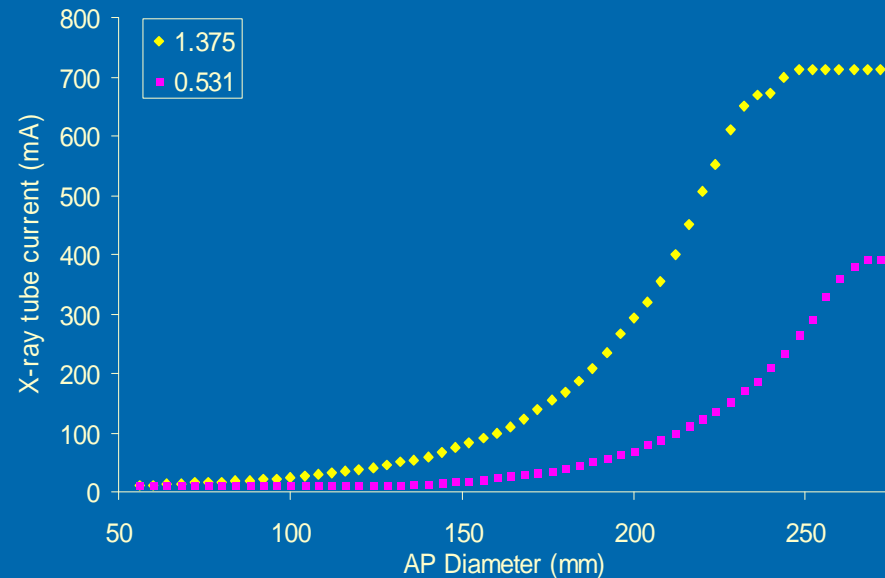
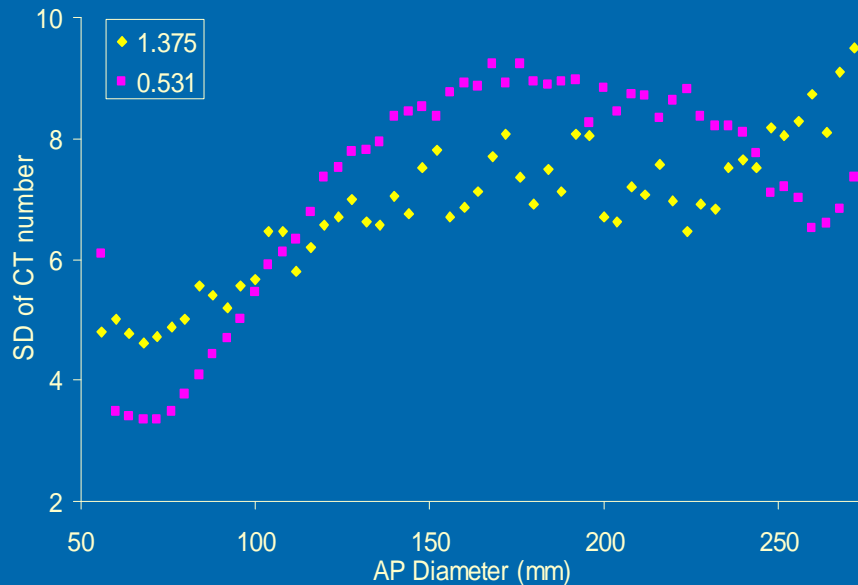
GIG  
CYMRU  
NHS  
WALES

Bwrdd Iechyd Prifysgol  
Caerdydd a'r Fro  
Cardiff and Vale  
University Health Board

14<sup>th</sup> October 2010

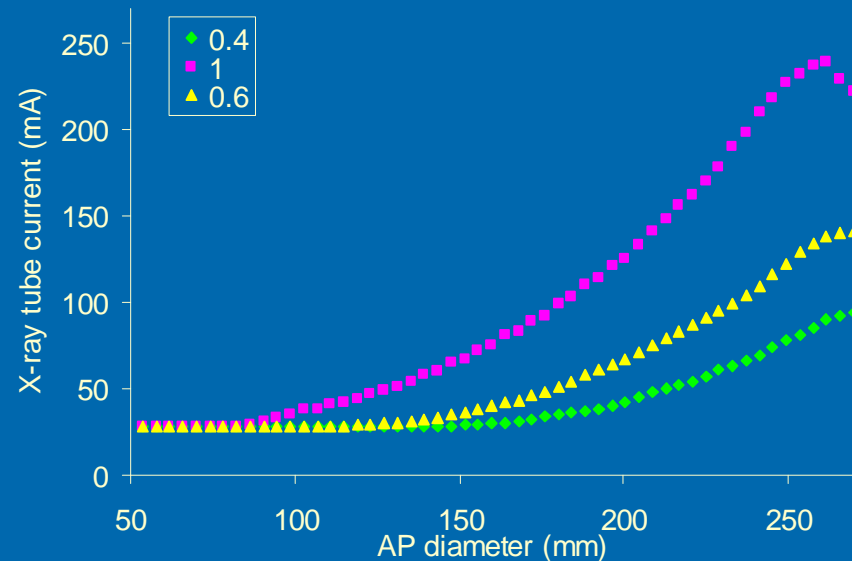
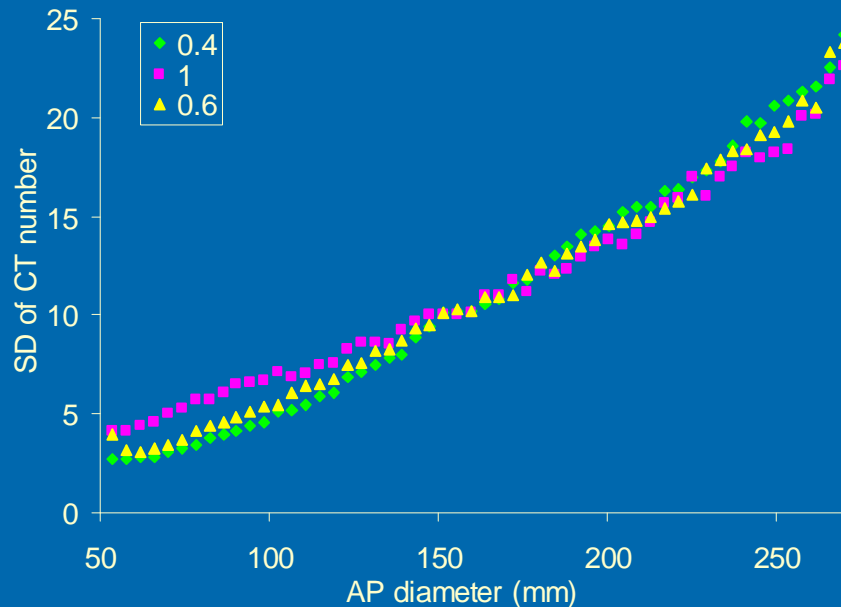


# Results - GE



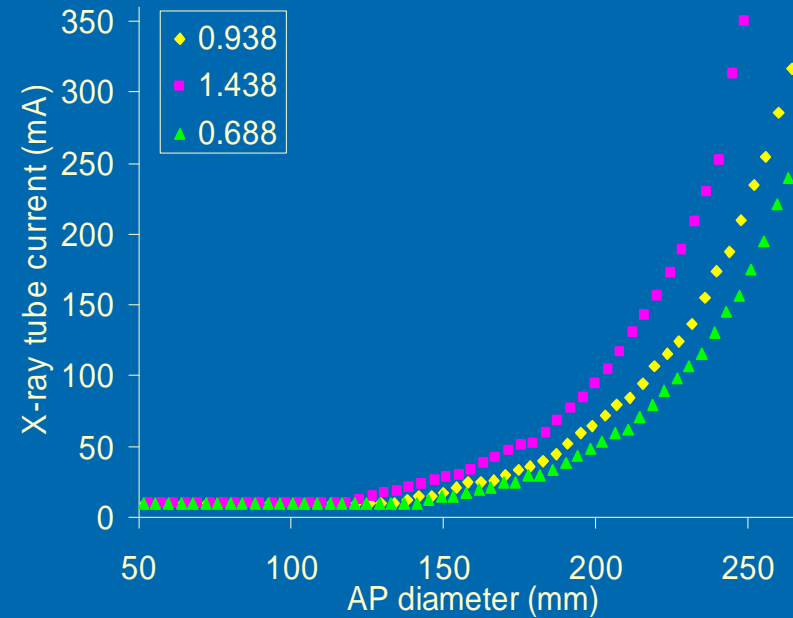
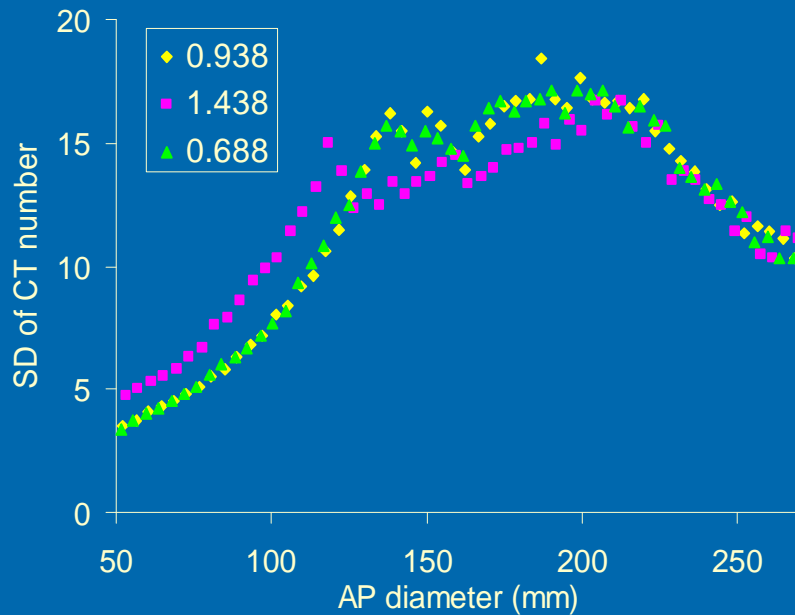
- Scan mode changed to helical with 40mm collimation to produce 5mm slices.
- Lowering pitch causes mA along the phantom to be reduced in order to achieve the NI specified.
- Reduced image noise between 100 and 250mm for increased pitch.

# Results - Siemens



- Changing pitch has a similar effect on GE, Siemens and Toshiba 64 slice scanners.
- Lowering pitch causes mA along the phantom to be reduced in order to achieve the image quality specified.

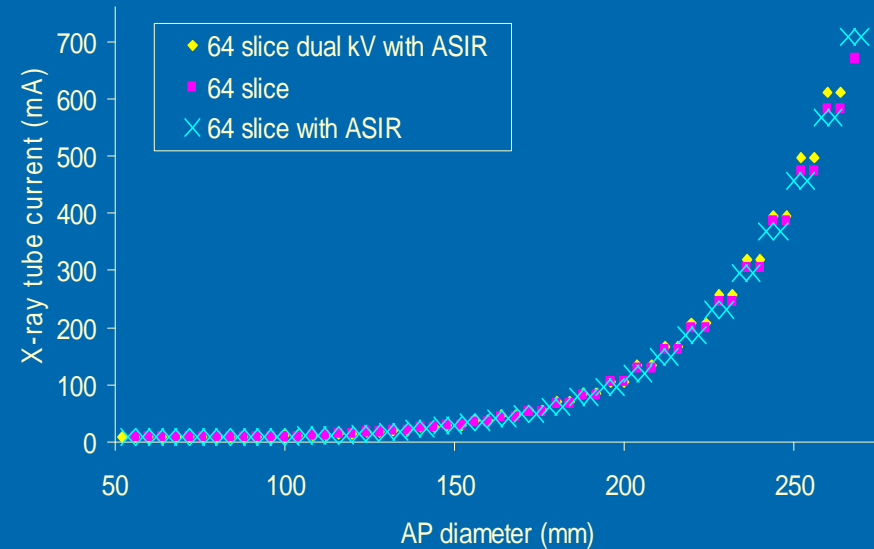
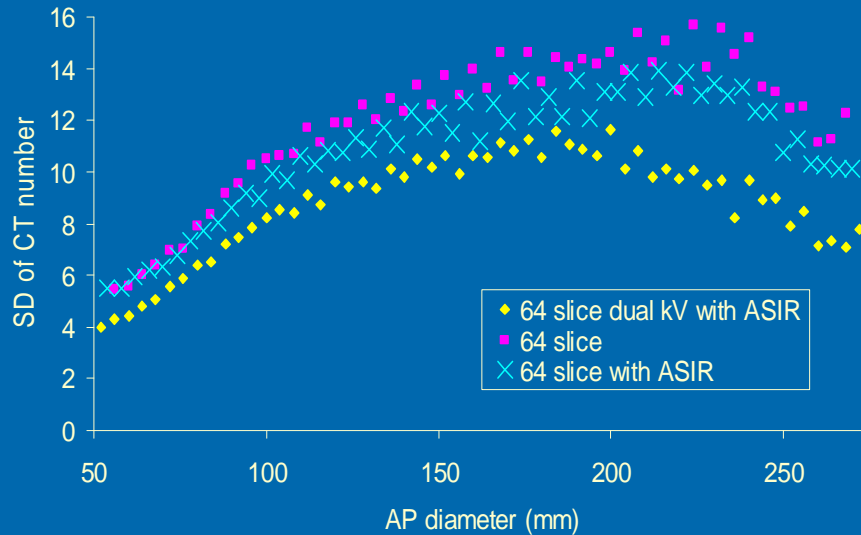
# Results - Toshiba



- Changing pitch has a similar effect on GE, Siemens and Toshiba 64 slice scanners.
- Lowering pitch causes mA along the phantom to be reduced in order to achieve the image quality specified.

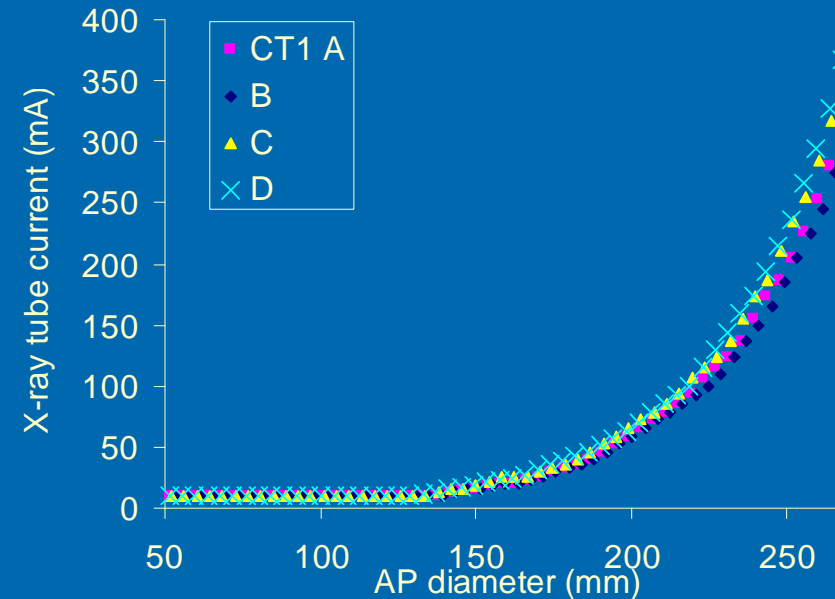
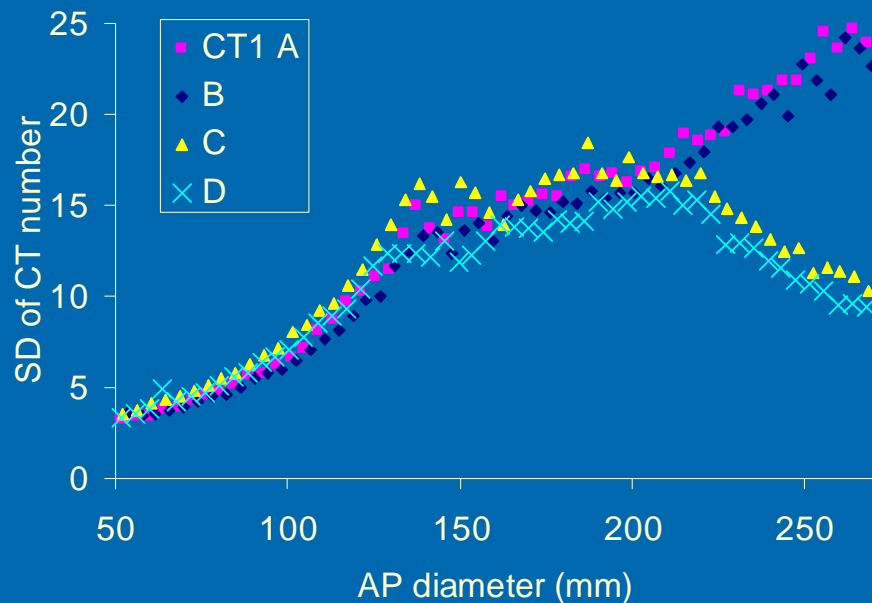
# Intra-manufacturer variation

# Results - GE



- Scanners with ASIR capabilities maintain image quality selected greater than the scanner without.
- The same mA modulation is apparent for the three scanners.

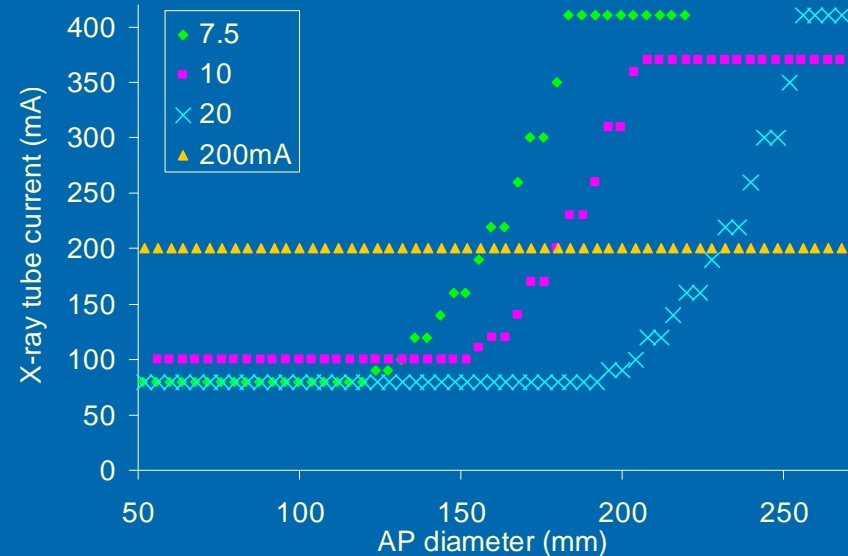
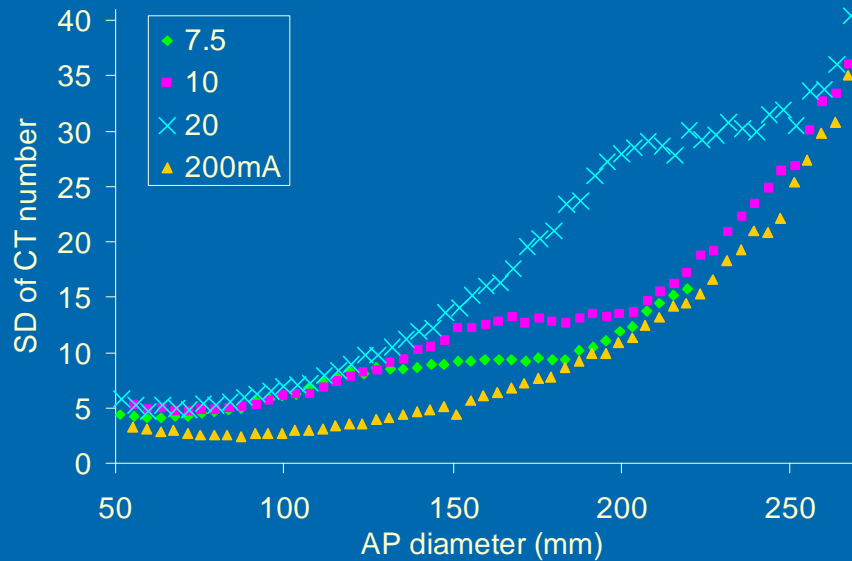
# Results - Toshiba



- Comparison of AEC system performance of four 64 slice Toshiba Aquilions.
- CT1 A and B behave differently to C and D with the same settings applied.
- C and D maintain greater image quality at increased AP diameters.

# Beware older scanners & software!

# Results - Toshiba



- Performance of 16 slice Toshiba was found to be different in respect to the Toshiba 64 slice scanners.
- Older software version, different AEC system interface.
- mA modulation only occurs over a small AP diameter range (~5cm).
- Point at which mA modulation occurs increases with AP diameter.



# Conclusion

- Scanners tested performed consistently with the findings described in the 2005 report by ImPACT<sup>1</sup>.
- Machines with apparently identical operation were found to have AEC systems which performed differently.
- Only through the individual testing of each scanner can the true behaviour of its AEC system be established.
- It is therefore essential that users operating each scanner fully understand not only how the relevant manufacturers AEC systems work in general but also how the specific scanner in their department operates.

<sup>1</sup> *CT scanner automatic exposure control systems*. Medicines and Healthcare Regulatory Agency, February 2005. Report 05016

Thank You



GIG  
CYMRU  
NHS  
WALES

Bwrdd Iechyd Prifysgol  
Caerdydd a'r Fro  
Cardiff and Vale  
University Health Board

14<sup>th</sup> October 2010