

# Development and initial experience of a detectability index plugin for ImageJ

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# Head and neck reconstruction filter

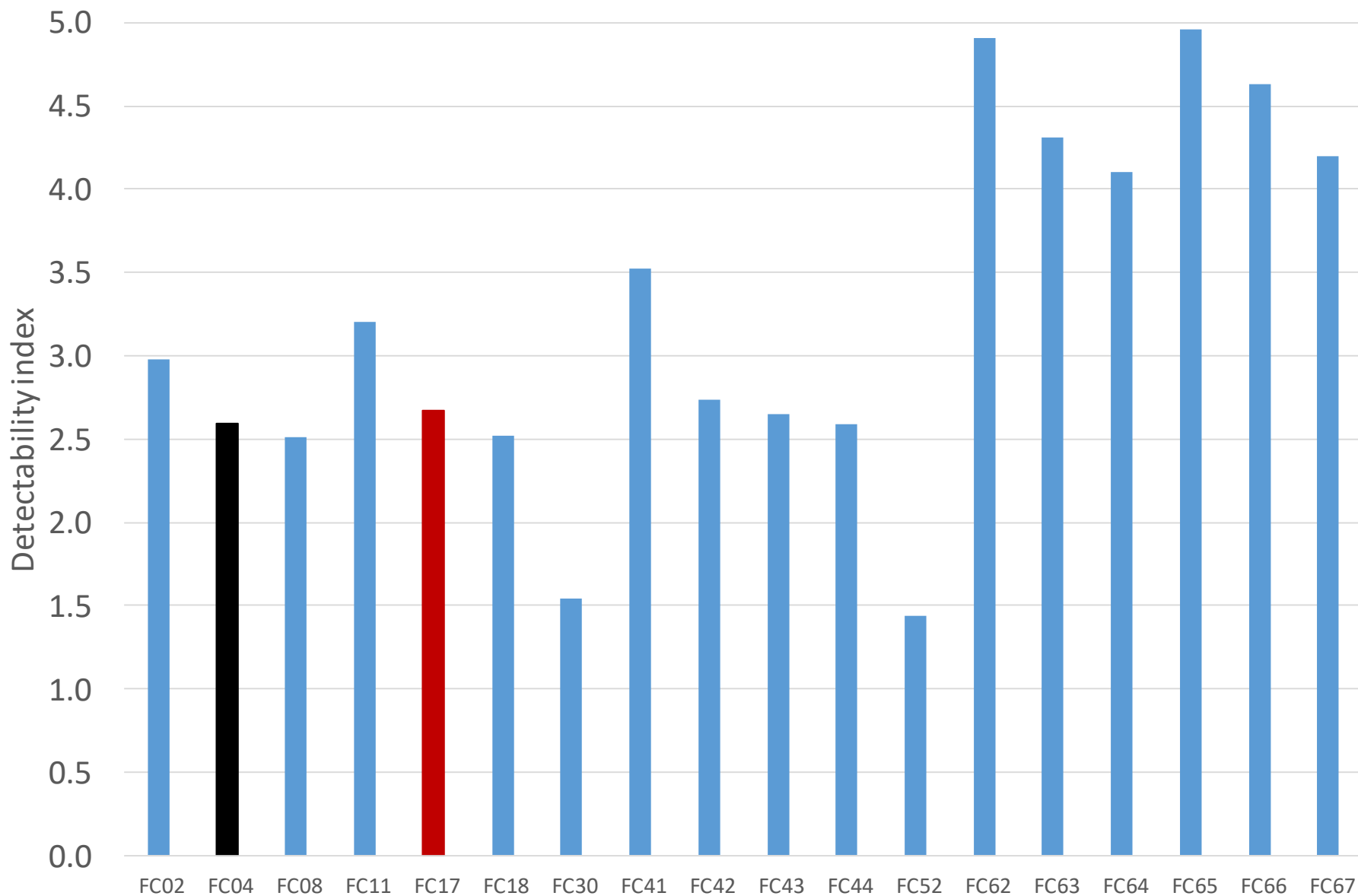
- Scanned Mercury 4.0 phantom<sup>1</sup> with clinical head and neck protocol
- Reconstructed with 18 different kernels
- Calculated detectability index ( $d'$ ) for each reconstruction
- Compared the values of  $d'$  for each kernel

# Head and neck reconstruction filter

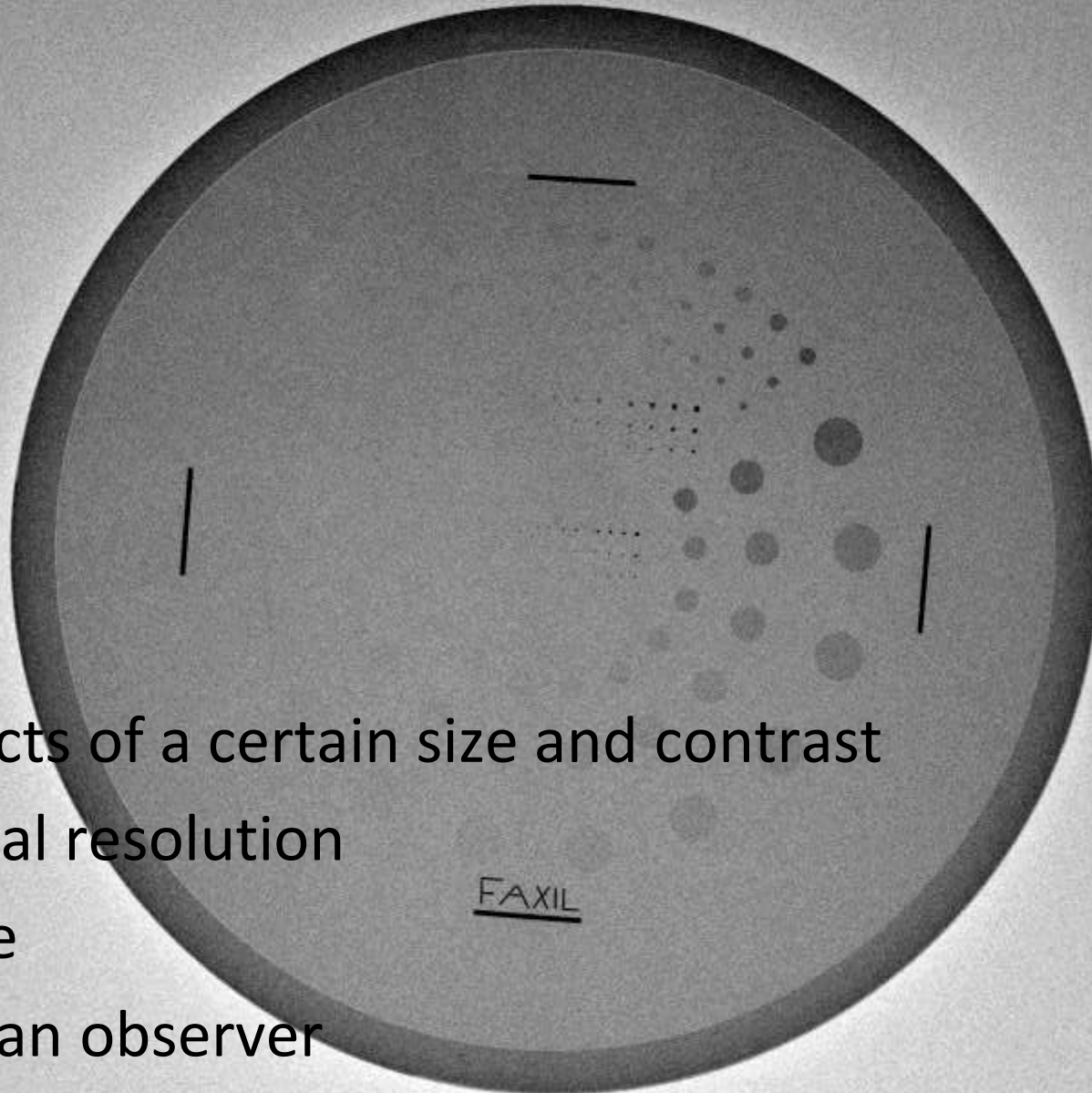
Filter	Clinical indication
FC02	Abdomen with beam hardening correction
FC04	
FC08	
FC11	Abdomen without beam hardening correction
FC17	
FC18	
FC30	Bone
FC41	Head without beam hardening correction
FC42	
FC43	
FC44	
FC52	Lung
FC62	Head with beam hardening correction
FC63	
FC64	
FC65	
FC66	
FC67	

Parameter	Value
Phantom section diameter	21 cm
Insert material	Polystyrene
Insert contrast (HU)	50
Simulated object diameter (mm)	5
Task function type	Disc
Image slices used for TTF calculation	66 – 76
Image slices used for NPS calculation	84 – 88
Eye model	Solomon et al. 2015

# Head and neck reconstruction filter



# Threshold contrast detectability



- Objects of a certain size and contrast
- Spatial resolution
- Noise
- Human observer

# Detectability index ( $d'$ )

$$d'^2 = \frac{\left[ \int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot E^2(f) df \right]^2}{\int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot \text{NPS}(f) \cdot E^4(f) df}$$

where

- $f$  is radial frequency
- $W(f)$  is a task function, the Fourier transform of the signal to be detected (object of a certain size and contrast)
- $\text{TTF}(f)$  is the task transfer function (spatial resolution)
- $\text{NPS}(f)$  is the noise power spectrum (noise)
- $E(f)$  is the frequency response of a model of the human eye (human observer)
- $f_N$  is the Nyquist frequency calculated from the image pixel size

$d'$  is a non-prewhitening with eye filter (NPWE) model observer adapted from [2](#)

Model observers similar to this have been shown to strongly correlate with:

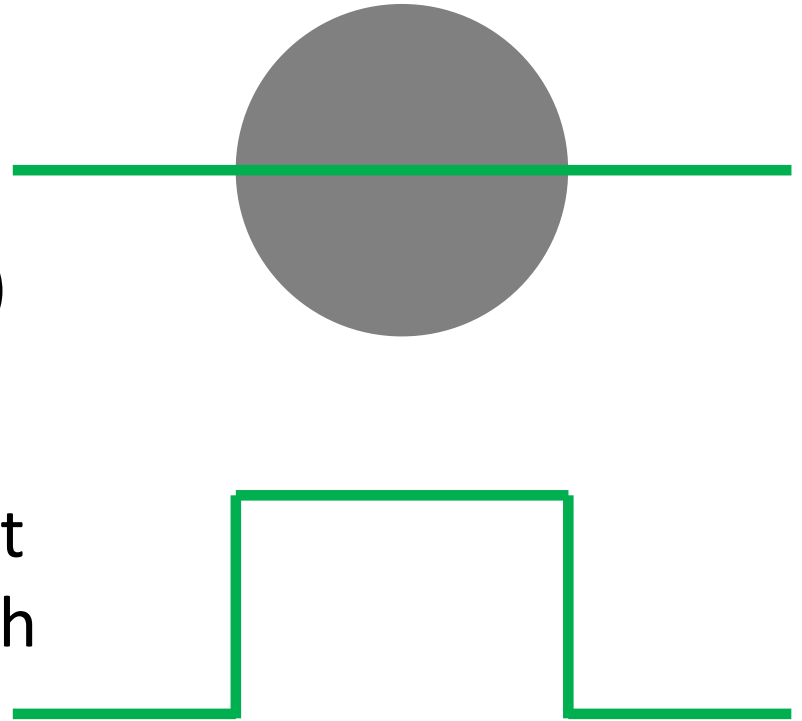
- human performance [3, 4, 5](#)
- threshold contrast in mammography and general radiography [6, 7](#)

# Other software for $d'$ calculation

- imQuest software<sup>8</sup> is available to calculate  $d'$  from images of the Mercury 4.0 phantom
  - Pre-compiled Matlab application
  - Source code also now available
- Issue with repeatability of  $d'$  calculation in pre-compiled version 7.0 of imQuest
  - Has been fixed in source code version
- Eye model and task function component results not readily available to the user
- Manual positioning of individual NPS regions

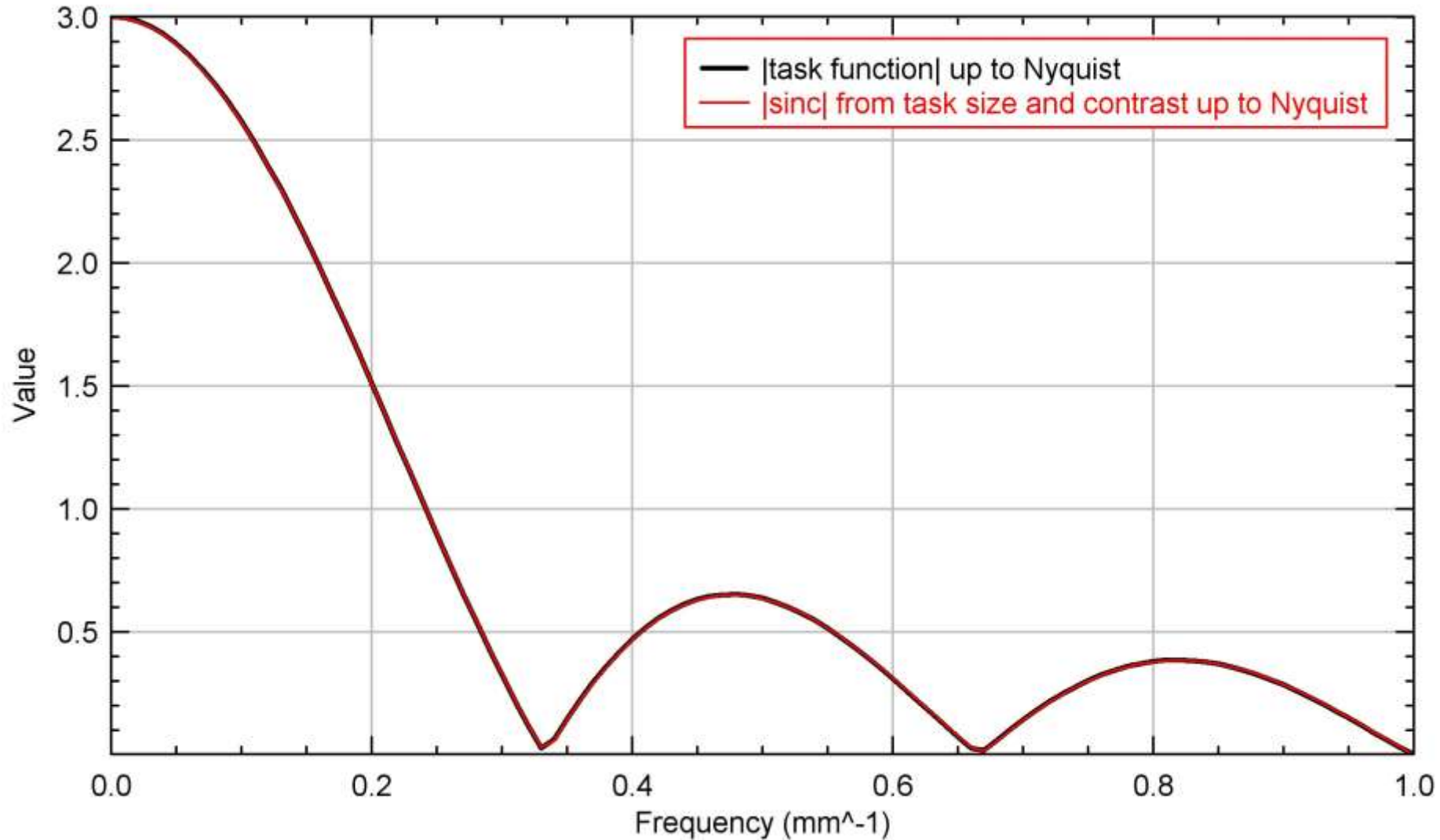
# Task function, $W(f)$

- The Fourier transform of the signal to be detected
- Signal is a “perfect” circular image that would result from CT scanning an infinite cylinder
  - specified diameter,  $d$
  - specified contrast,  $c$
- Has radial symmetry (a circle)
- “Top-hat” in cross-section
- Fourier transform of a top-hat function is a sinc function with maximum value =  $c \cdot d$  <sup>9</sup>





# Task function, $W(f)$



# Eye function, $E(f)$

- Simple model incorporating the frequency response of the human eye; several versions [2](#), [3](#), [4](#), [10](#)

# Eye function, $E(f)$

Solomon et al <sup>2</sup> use:

$$E(\rho) = \left| \eta \cdot \rho^{a_1} \cdot e^{-a_2 \cdot \rho^{a_3}} \right|^2$$

where

$\rho$  is angular spatial frequency ( $\text{deg}^{-1}$ )

$a_1 = 1.5$ ;  $a_2 = 0.98$ ;  $a_3 = 0.68$

$\eta$  is a factor to set  $E(\rho)_{\max}$  to 1.0

# Eye function, $E(f)$

Angular spatial frequency ( $\rho$ ) calculated using:

$$\rho = f \times \frac{FOV \cdot R \cdot \pi}{D \cdot 180}$$

where

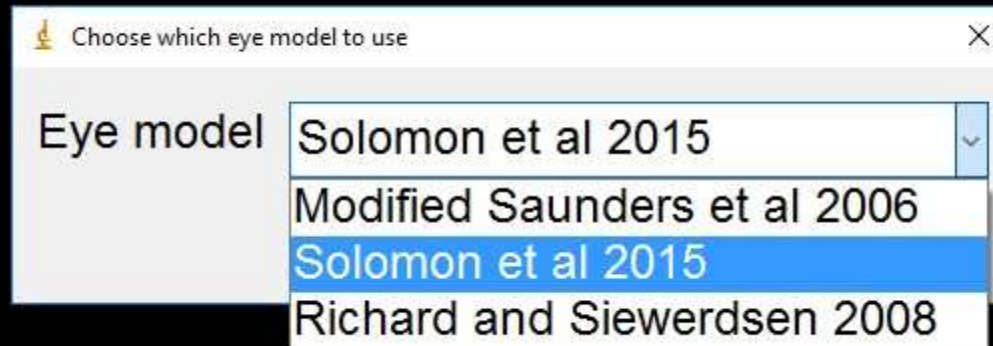
$f$  is radial spatial frequency ( $\text{mm}^{-1}$ )

FOV is the reconstructed field of view of the image (mm)

$R$  is the viewing distance (mm)

$D$  is the size of the displayed image on the screen (mm)

# Example eye function, $E(f)$

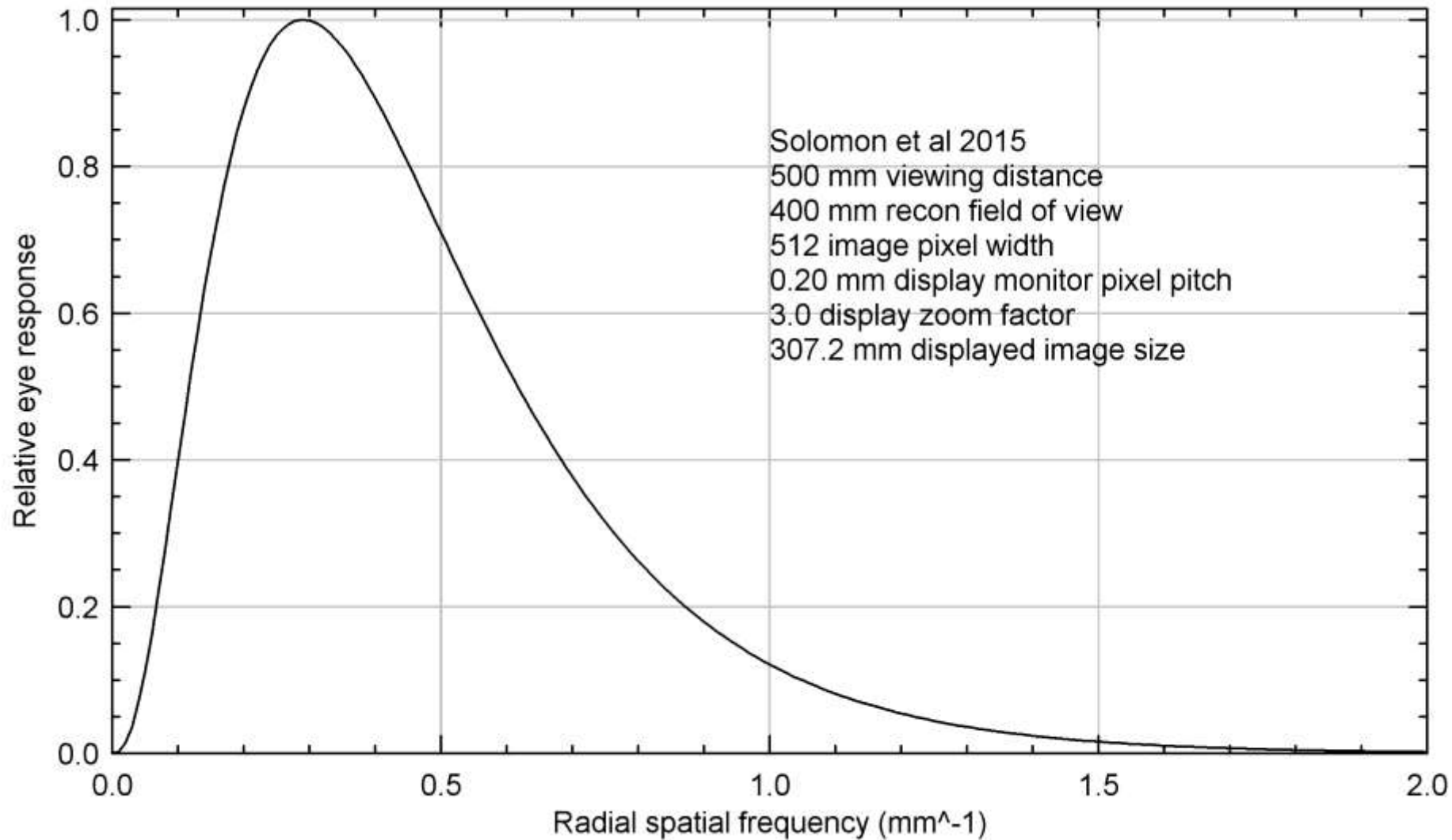


# Example eye function, $E(f)$

Solomon et al 2015 options

Radial spatial frequency cutoff ( $\text{mm}^{-1}$ )	<input type="text" value="2.00"/>
Radial spatial frequency increment ( $\text{mm}^{-1}$ )	<input type="text" value="0.01"/>
Viewing distance (mm)	<input type="text" value="500"/>
Image reconstructed field of view (mm)	<input type="text" value="400"/>
Physical image size on the display monitor:	
Display pixel pitch (mm)	<input type="text" value="0.20"/>
Display zoom factor	<input type="text" value="3.0"/>
Image pixel width	<input type="text" value="512"/>

# Example eye function, $E(f)$

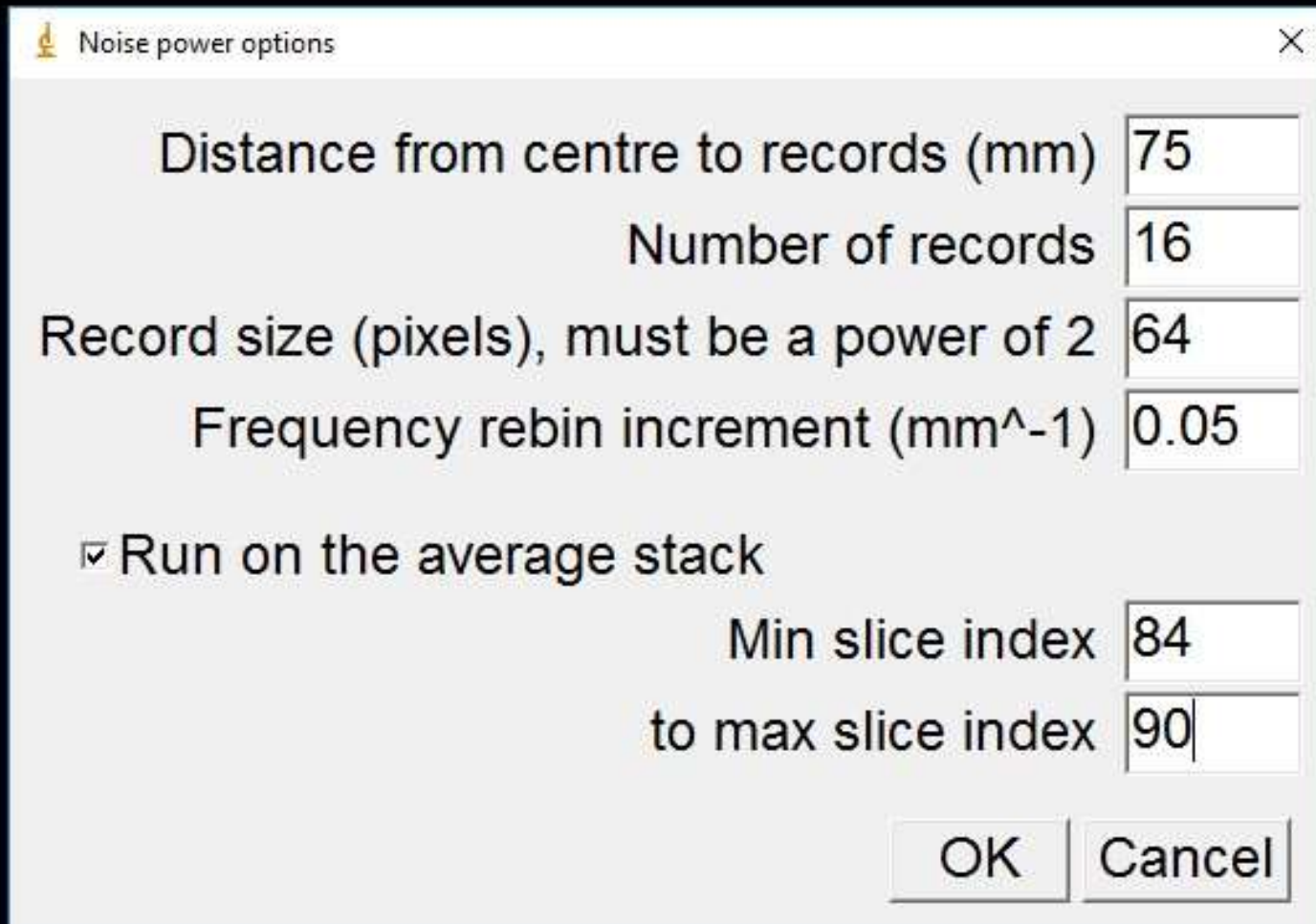


# Noise power spectrum, NNPS (f)

- Calculated from a number of square “records” positioned a specified radial distance from the centre of an ROI or the whole image
- 2D version of ICRU 87 method <sup>11</sup>
- Configurable:
  - Number of records
  - Size of records
  - Radial distance
  - Number of images to use



# Noise power spectrum, NNPS (f)

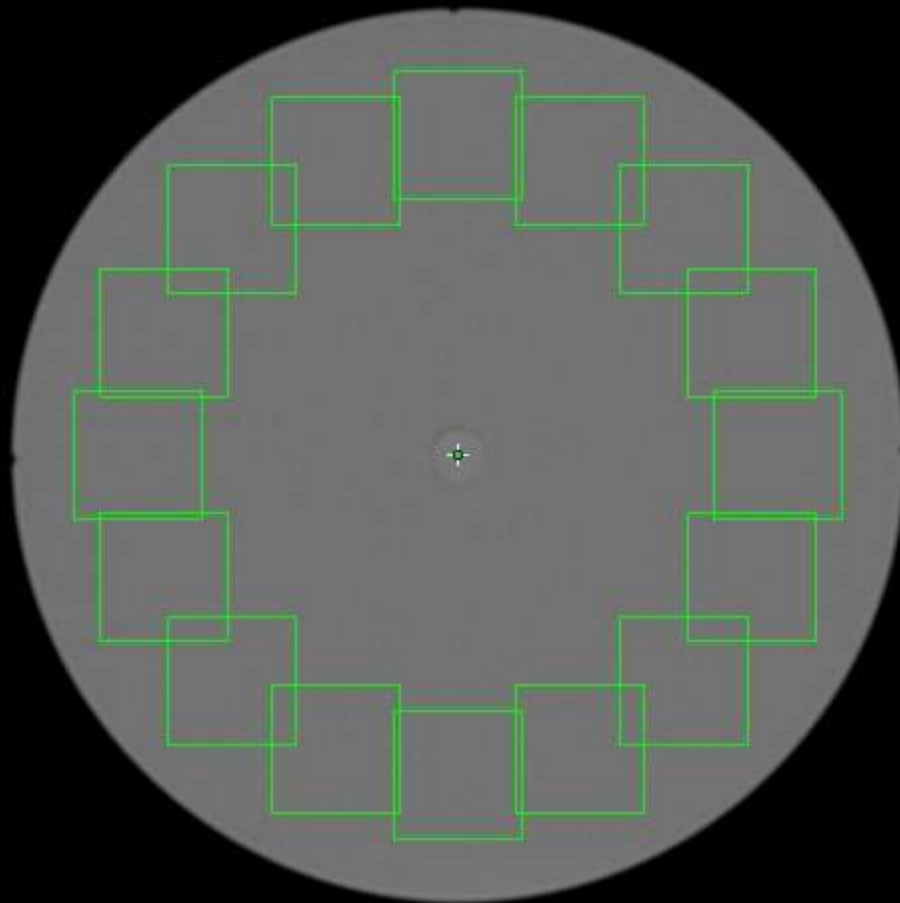


A screenshot of a software dialog box titled "Noise power options". The dialog box contains several input fields and a checkbox. The fields are: "Distance from centre to records (mm)" with a value of 75, "Number of records" with a value of 16, "Record size (pixels), must be a power of 2" with a value of 64, and "Frequency rebin increment (mm<sup>-1</sup>)" with a value of 0.05. There is a checked checkbox labeled "Run on the average stack". Below the checkbox are two more input fields: "Min slice index" with a value of 84 and "to max slice index" with a value of 90. At the bottom right of the dialog box are two buttons: "OK" and "Cancel".

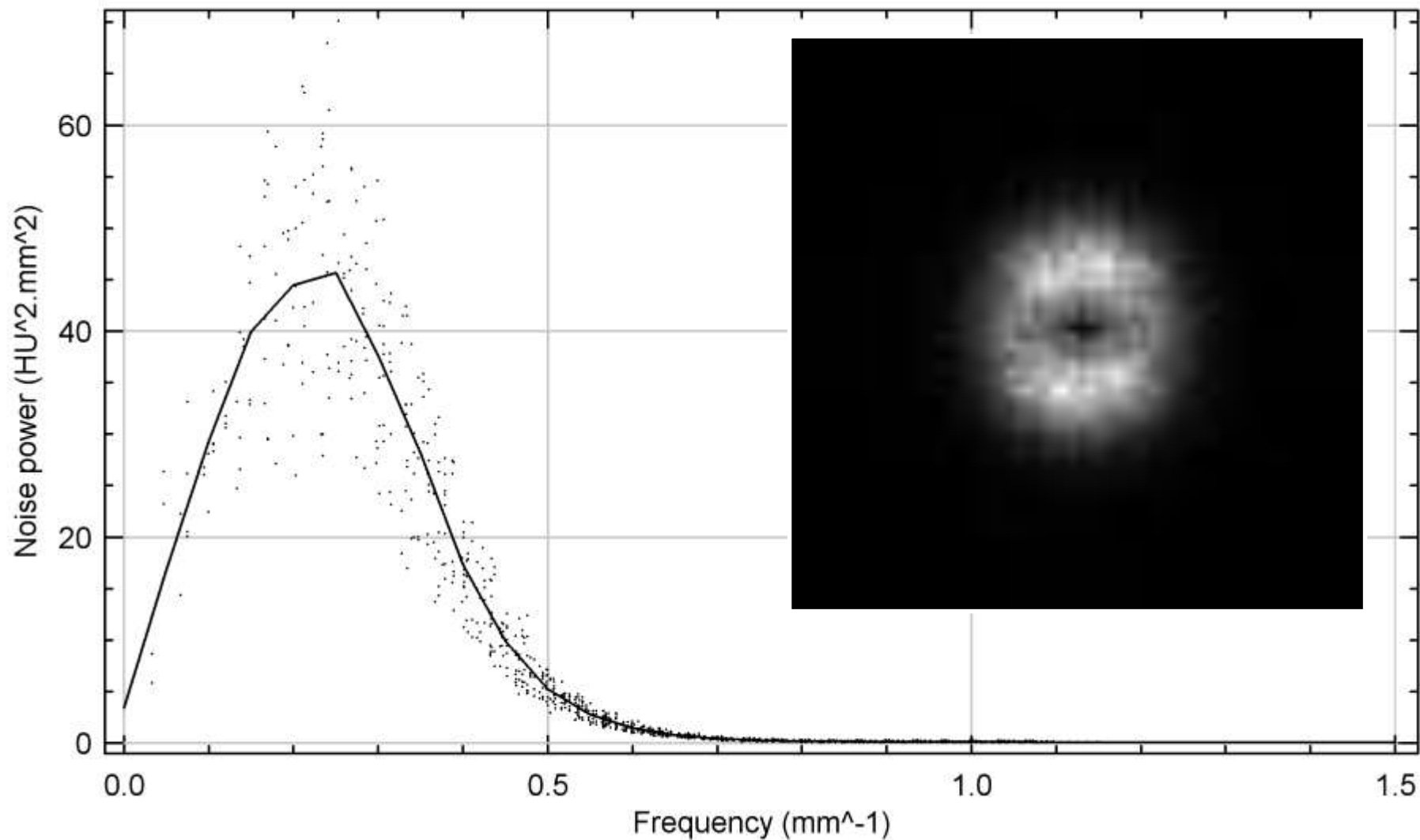
Distance from centre to records (mm)	75
Number of records	16
Record size (pixels), must be a power of 2	64
Frequency rebin increment (mm <sup>-1</sup> )	0.05
<input checked="" type="checkbox"/> Run on the average stack	
Min slice index	84
to max slice index	90

OK Cancel

# Noise power spectrum, NNPS (f)



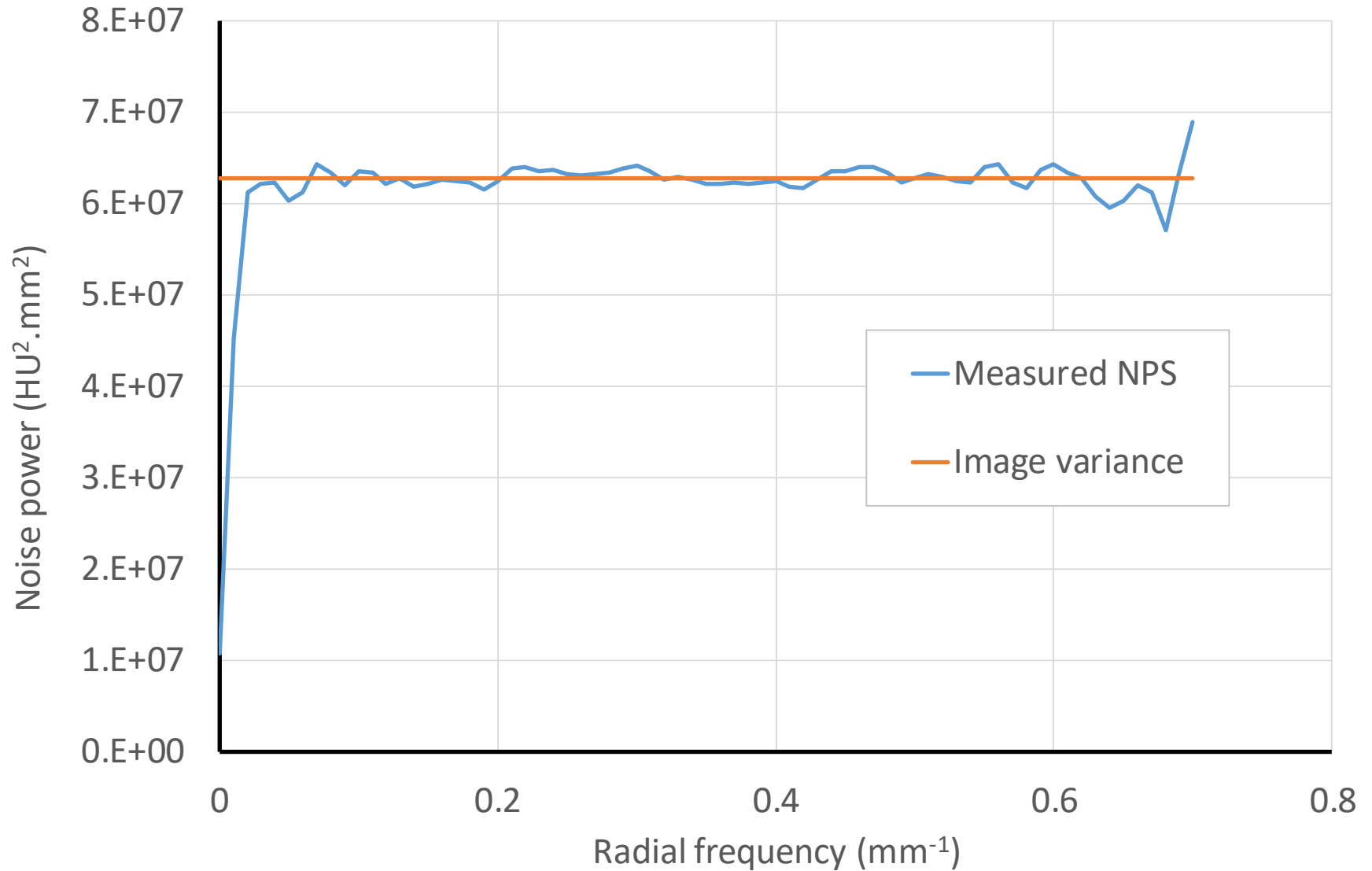
# Noise power spectrum, NNPS (f)



# Noise power spectrum, NNPS (f)

- Validation
  - Random noise image created in ImageJ
  - 1024 x 1024; 1 mm pixel size
  - Ran NPS plugin (32 records, 128 pixel record size, 350 mm record radius)
  - Measured the variance of the image
  - Noise power should be equal to variance

# Noise power spectrum, NNPS (f)



# Task transfer function, TTF(f)

- Similar to the modulation transfer function (MTF) but suited to non-linear systems that may depend on the imaging task <sup>12</sup>
- Fourier transform of the line-spread function of an object with a certain contrast and noise

# Task transfer function, TTF(f)

Task transfer function options

Object diameter (mm) [Mercury 25, Catphan 12]

Pixel reduction factor

Frequency rebin increment (mm<sup>-1</sup>)

Find centre of mass

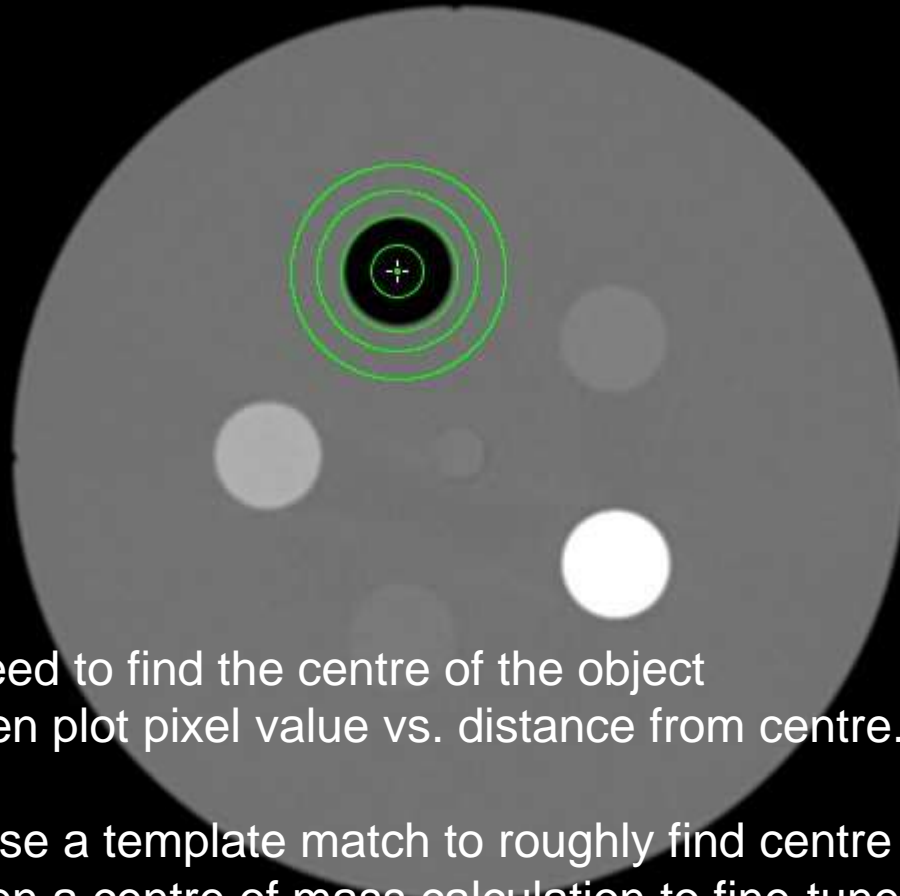
Show advanced options

Run on the average stack

Min slice index

to max slice index

# Task transfer function, $TTF(f)$

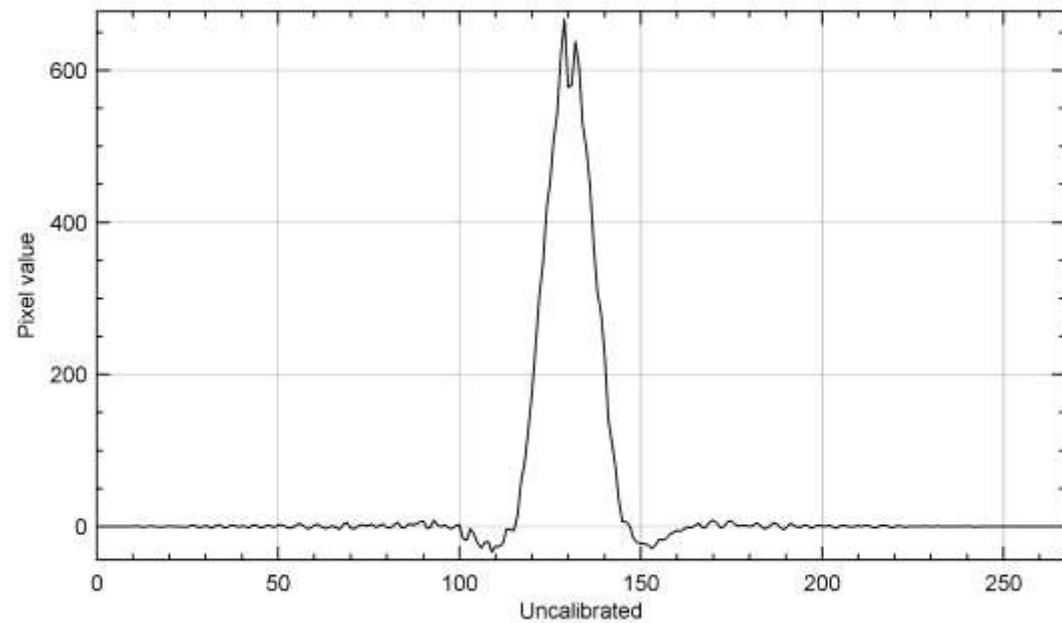
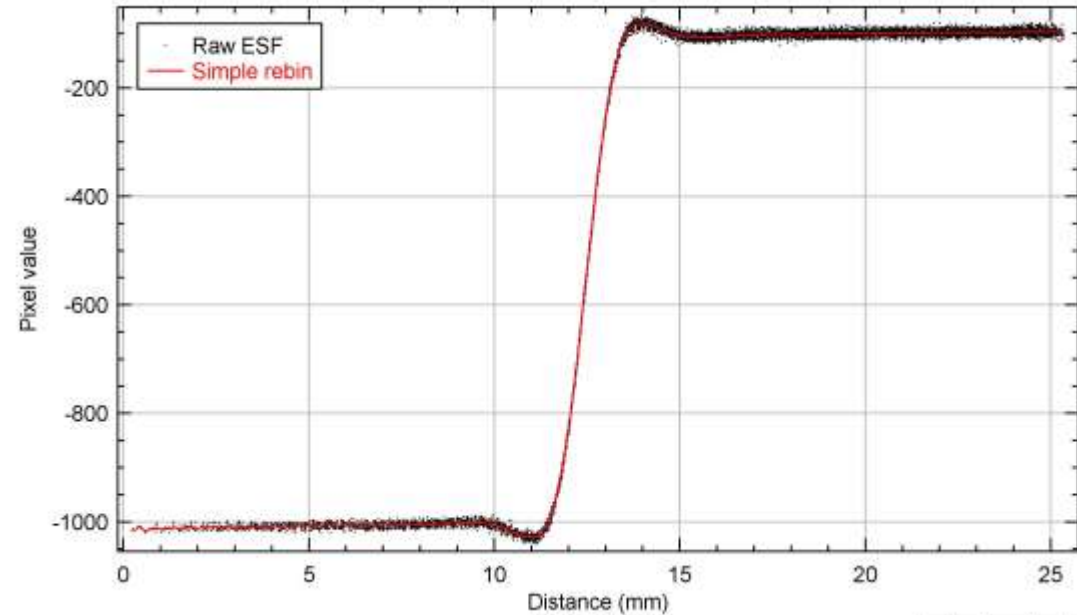


Need to find the centre of the object  
then plot pixel value vs. distance from centre.

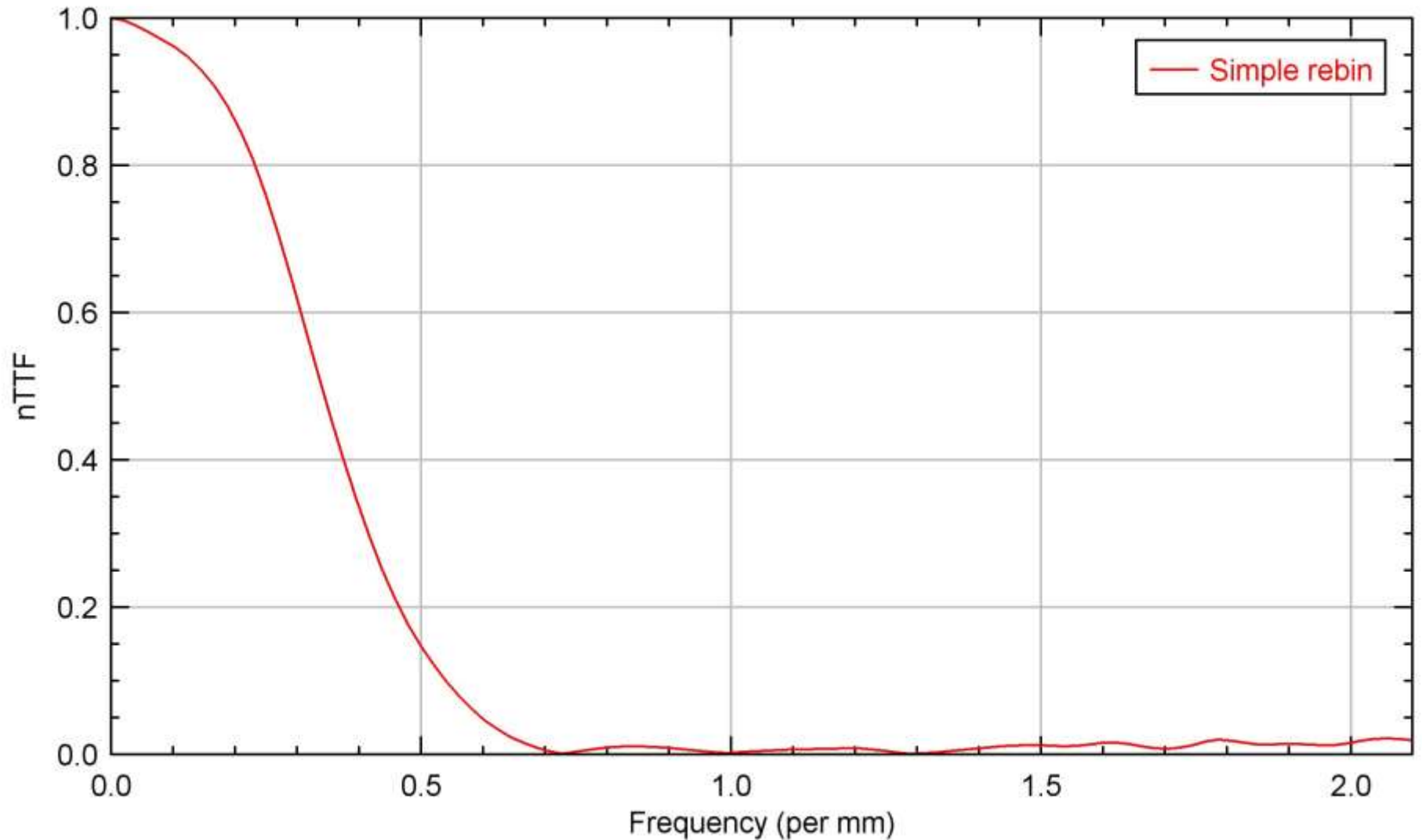
I use a template match to roughly find centre  
then a centre of mass calculation to fine-tune



# Task transfer function, TTF(f)



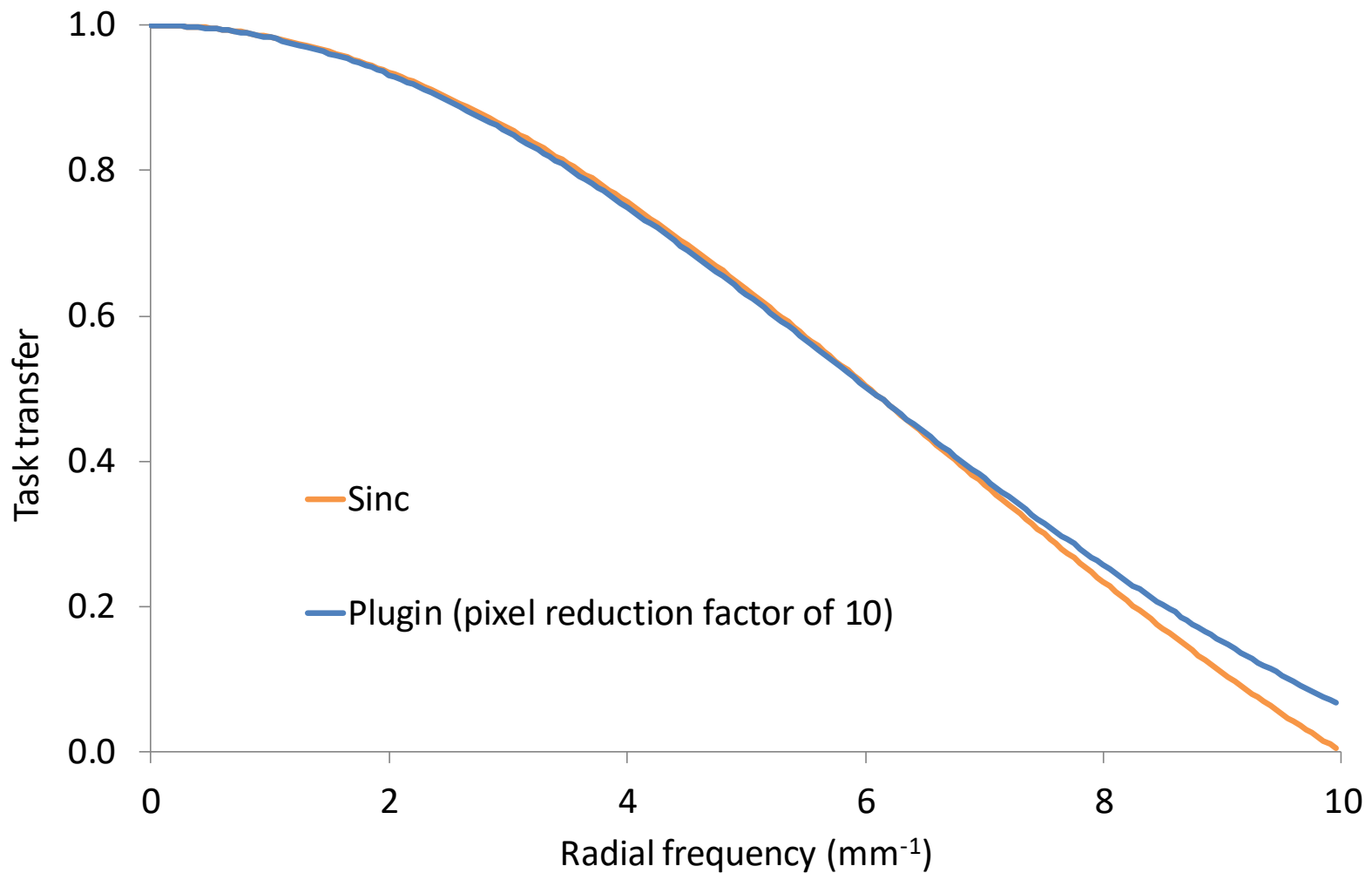
# Task transfer function, TTF(f)



# Task transfer function, TTF(f)

- Validation
  - Creation of a “perfect” test image
  - Should have a TTF equal to the sinc function calculated from the image pixel size

# Task transfer function, TTF(f)



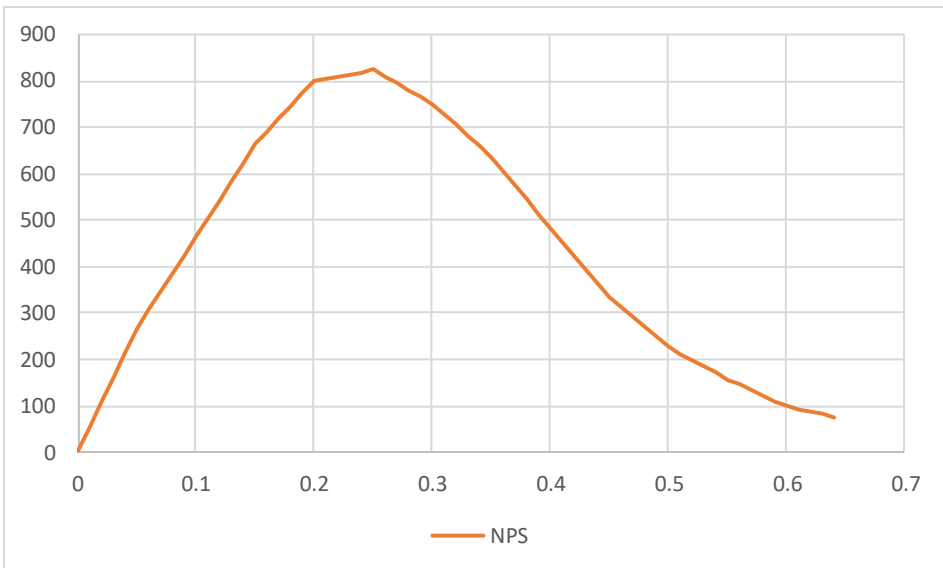
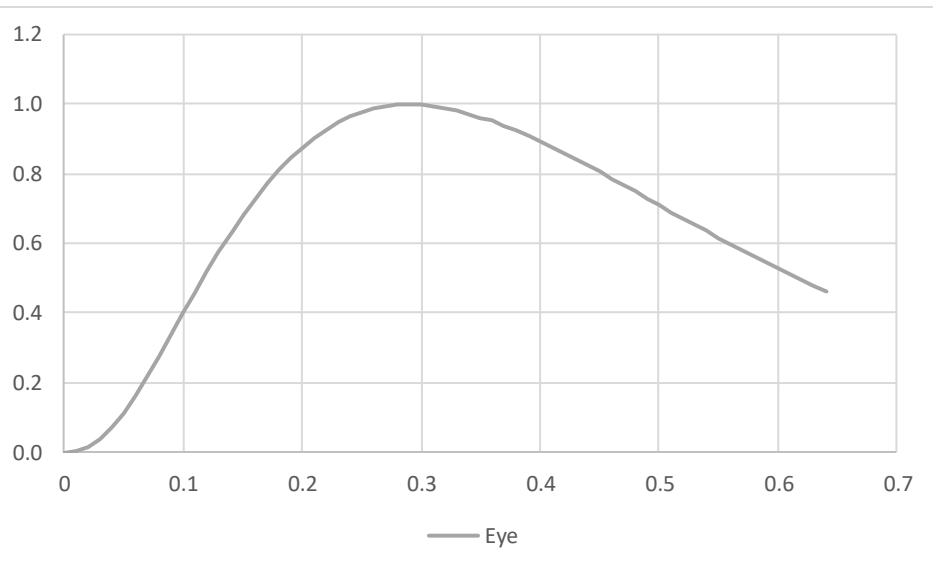
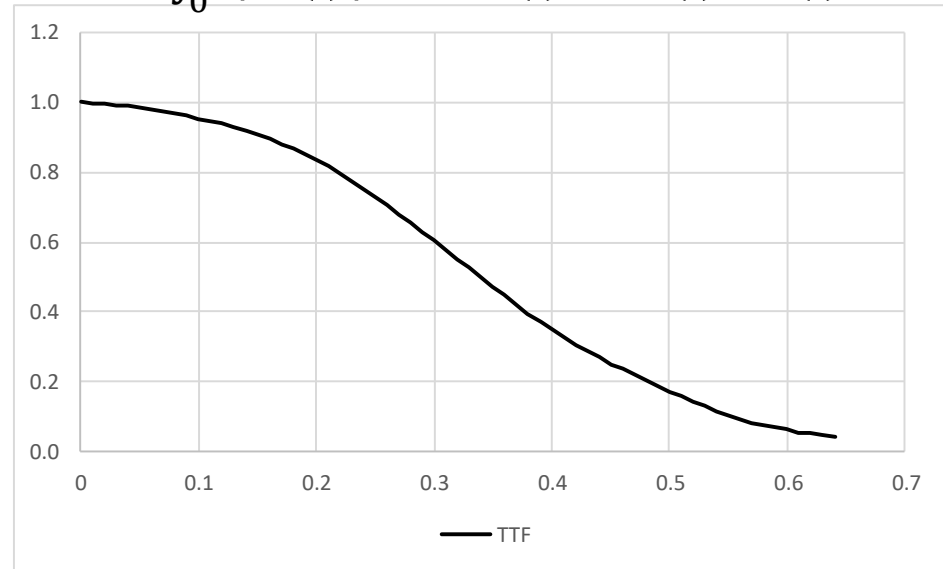
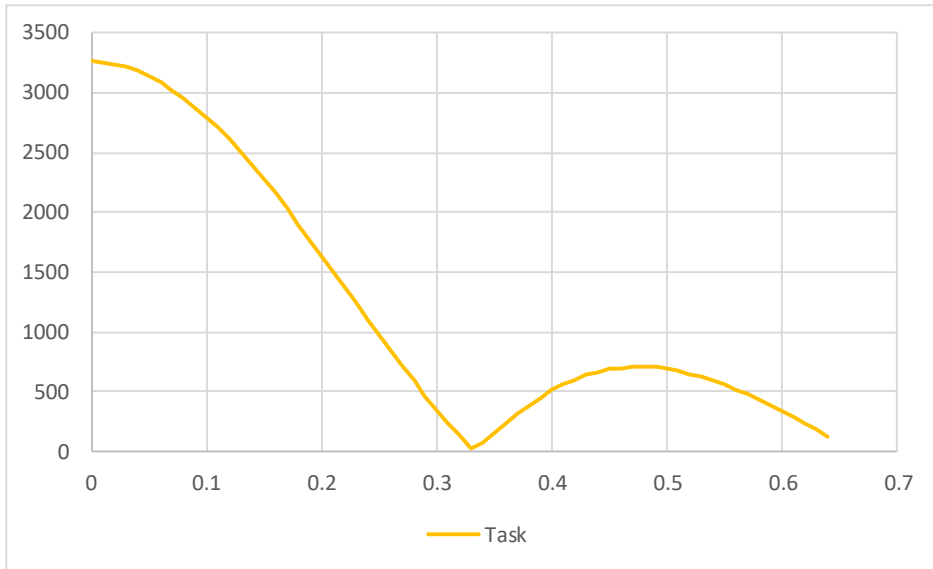
# Calculation of $d'$

- Multiply the components together and integrate over radial frequency as per:

$$d'^2 = \frac{\left[ \int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot E^2(f) \, df \right]^2}{\int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot \text{NPS}(f) \cdot E^4(f) \, df}$$

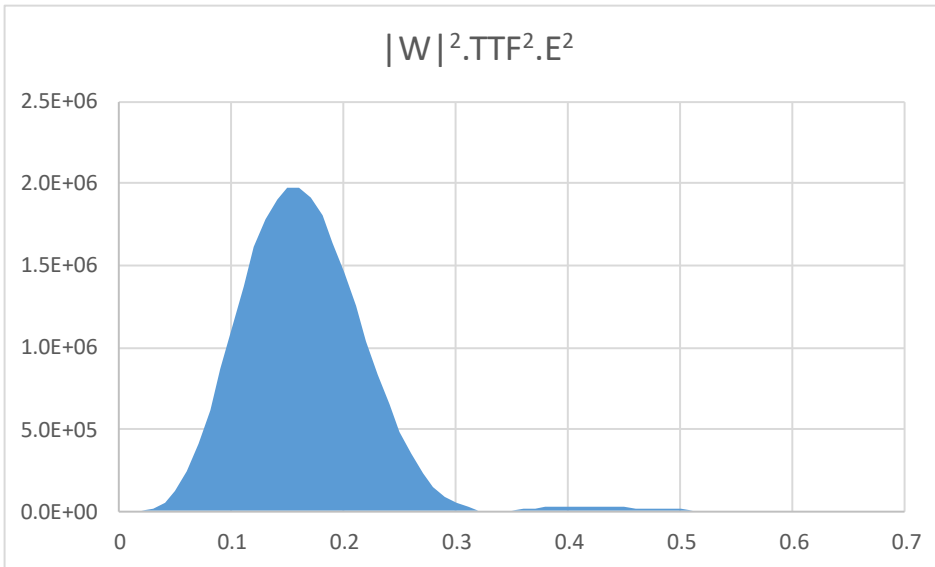
# Calculation of $d'$

$$d'^2 = \frac{\left[ \int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot E^2(f) df \right]^2}{\int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot \text{NPS}(f) \cdot E^4(f) df}$$

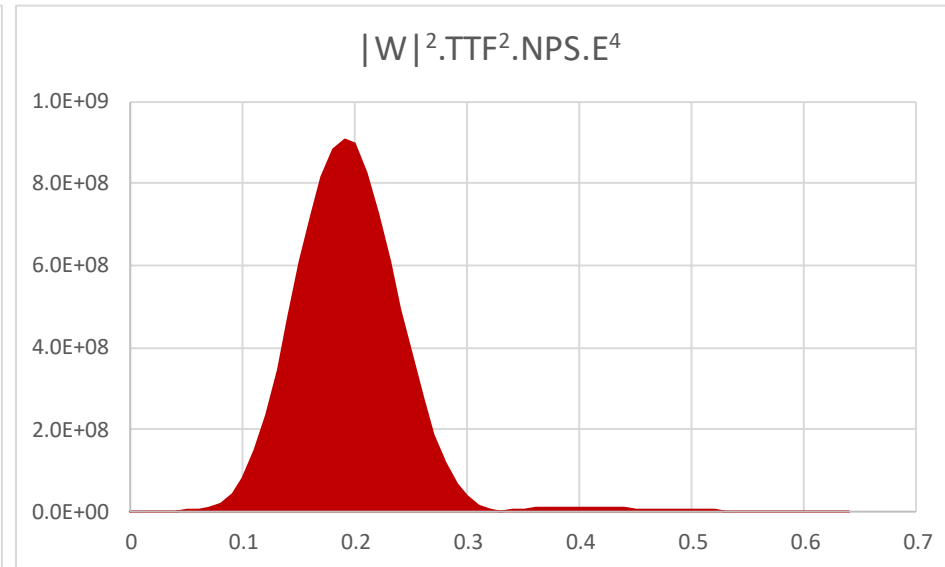


# Calculation of $d'$

$$d'^2 = \frac{\left[ \int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot E^2(f) df \right]^2}{\int_0^{f_N} |W(f)|^2 \cdot \text{TTF}^2(f) \cdot \text{NPS}(f) \cdot E^4(f) df}$$



263,126



100,129,054

$$d' = \frac{263,126}{\sqrt{100,129,054}} = 26.3$$

# On-going work

- We plan to embed  $d'$  in our CT optimisation work
- We are currently using  $d'$  to compare chest CT protocols across the Trust



# Summary

- Written a series of ImageJ plugins to calculate detectability index ( $d'$ )
  - $d'$  correlates well with human observers <sup>3, 4, 5</sup> and threshold contrast <sup>6, 7</sup>
- Used JetBrains IntelliJ IDEA development environment for the programming <sup>14</sup>
- Used Apache Commons Math library v3.6.1 <sup>15</sup>
- Used Bitbucket for source code management <sup>16</sup>
- Simple validation carried out on each  $d'$  component
- $d'$  calculated from images of a Mercury 4.0 phantom <sup>1</sup> to help identify an optimal reconstruction filter for head and neck scans on a CT simulator

# Plugin availability

- My source code is on Bitbucket here:
  - <https://bitbucket.org/dplatten/imagej-plugins/>
  - Download the source code and look in the Javadoc folder for html documentation; there are also comments in the source files
- Compiled jar files are on Bitbucket in the above repository:
  - <https://bitbucket.org/dplatten/imagej-plugins/src/e6da6c90b1b13ba1d9139cfbaf744b72e8ae2c89/project-intellij/jars/>
  - Download QuantitativeIQ.jar and put it in the ImageJ plugins folder
  - Put the commons-math3-3.6.1.jar file somewhere where your Java virtual machine can find it, such as:
    - C:\Program Files\Java\jre1.8.0\_202\lib\ext
    - It may work if you put it in your ImageJ plugins folder

# References

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3. Richard, S. and Siewerdsen, J.H. (2008). Comparison of model and human observer performance for detection and discrimination tasks using dual-energy x-ray images: Model and human observer performance in dual-energy imaging. *Medical Physics*, 35(11), pp.5043–5053, <https://doi.org/10.1118/1.2988161>
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5. Solomon, J. et al. (2015). Diagnostic Performance of an Advanced Modeled Iterative Reconstruction Algorithm for Low-Contrast Detectability with a Third-Generation Dual-Source Multidetector CT Scanner: Potential for Radiation Dose Reduction in a Multireader Study. *Radiology*, 275(3), pp.735–745, <https://doi.org/10.1148/radiol.15142005>.
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10. Saunders, R.S. and Samei, E. (2006). Resolution and noise measurements of five CRT and LCD medical displays: Resolution and noise of medical displays. *Medical Physics*, 33(2), pp.308–319 <https://doi.org/10.1118/1.2150777>
11. Boone, J.M. et al. (2012). ICRU Report No. 87 Radiation dose and image-quality assessment in computed tomography. *Journal of the ICRU*, 12(1), <https://doi.org/10.1093/jicru/ndt006>
12. Chen, B. et al. (2014). Assessment of volumetric noise and resolution performance for linear and nonlinear CT reconstruction methods: Assessing CT noise and resolution for nonlinear reconstruction. *Medical Physics*, 41(7), p.071909, <https://doi.org/10.1148/10.1118/1.4881519>
13. Christianson, O. et al. (2015). An Improved Index of Image Quality for Task-based Performance of CT Iterative Reconstruction across Three Commercial Implementations. *Radiology*, 275(3), pp.725–734, <https://doi.org/10.1148/radiol.15132091>
14. JetBrains IntelliJ IDEA, <http://www.jetbrains.com/idea/>
15. Apache Commons Math library v3.6.1, <http://commons.apache.org/proper/commons-math/>
16. Bitbucket, <https://bitbucket.org/>

# Conversion from image spatial frequency ( $\text{mm}^{-1}$ ) to image angular spatial frequency ( $\text{deg}^{-1}$ )

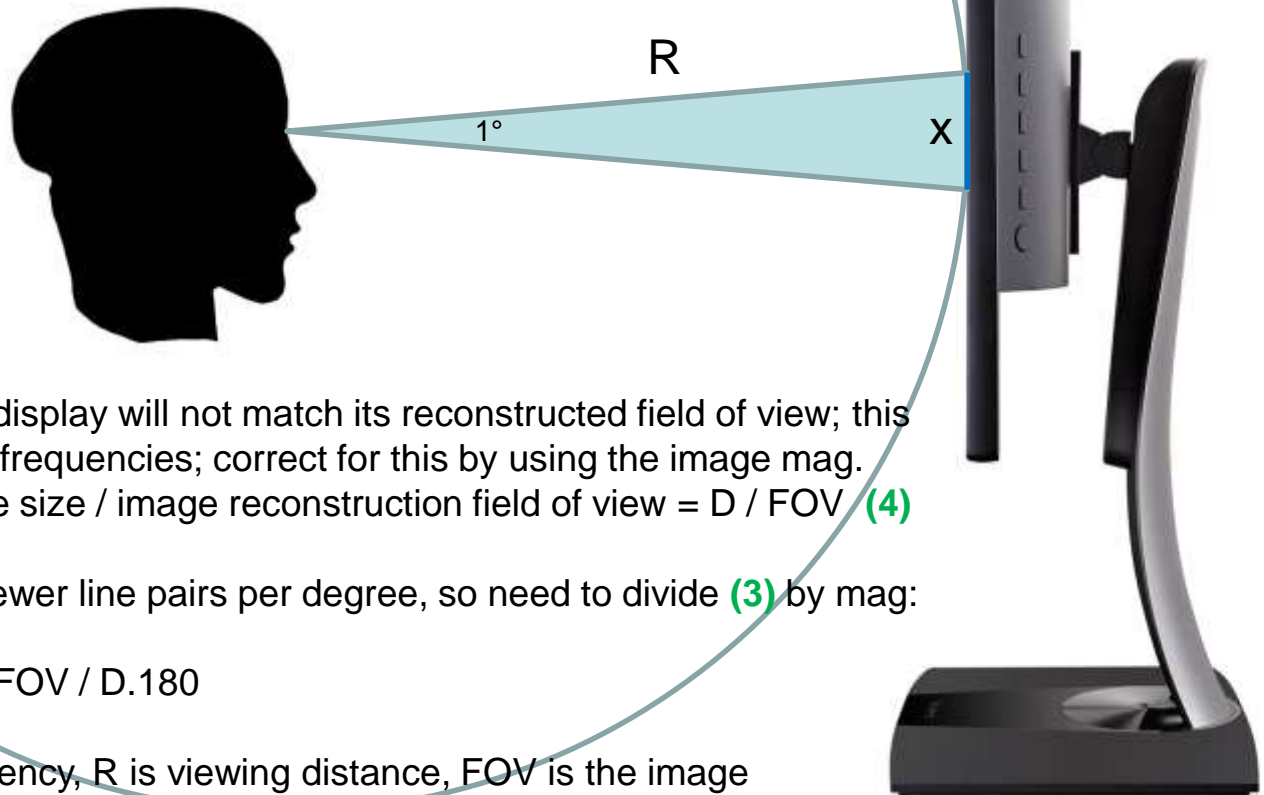
Circumference  $C = 2 \cdot \pi \cdot R$

Distance  $x$  is approximately  $C / 360 = 2 \cdot \pi \cdot R / 360 = \pi \cdot R / 180$  (1)

$f$  = spatial frequency

Line pairs in distance corresponding to  $1^\circ$  = angular spatial frequency ( $\rho$ ) =  $f \cdot x$  (2)

Substitute (1) into (2):  $\rho = f \cdot \pi \cdot R / 180$  (3)



The size of the image on the display will not match its reconstructed field of view; this changes the apparent spatial frequencies; correct for this by using the image mag.

Image mag = displayed image size / image reconstruction field of view =  $D / \text{FOV}$  (4)

As mag increases there are fewer line pairs per degree, so need to divide (3) by mag:

$$\rho = f \cdot \pi \cdot R / 180 / \text{mag} = f \cdot \pi \cdot R \cdot \text{FOV} / D \cdot 180$$

where  $f$  is image spatial frequency,  $R$  is viewing distance,  $\text{FOV}$  is the image reconstruction field of view and  $D$  is the size of the image on the display screen

Thanks for listening

Any questions?