

Optimisation and standardisation of CT imaging post microwave liver ablation

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The Royal Marsden Hospital, London

CT Users Group meeting
October 2023

Context: Microwave liver ablation

- Thermal ablation has become an accepted treatment strategy for primary and oligometastatic secondary liver cancer.

Needles are placed from the skin directly into a target liver tumour

Lethal microwave energy deposited

Tumour must be fully heated with a margin of normal tissue (safety margin)

Advantages:

Lower cost

Shorter hospital stays



Lower morbidity and mortality than surgery

Disadvantages:

High recurrence rate

Often only used for inoperable tumours

Context: Microwave liver ablation

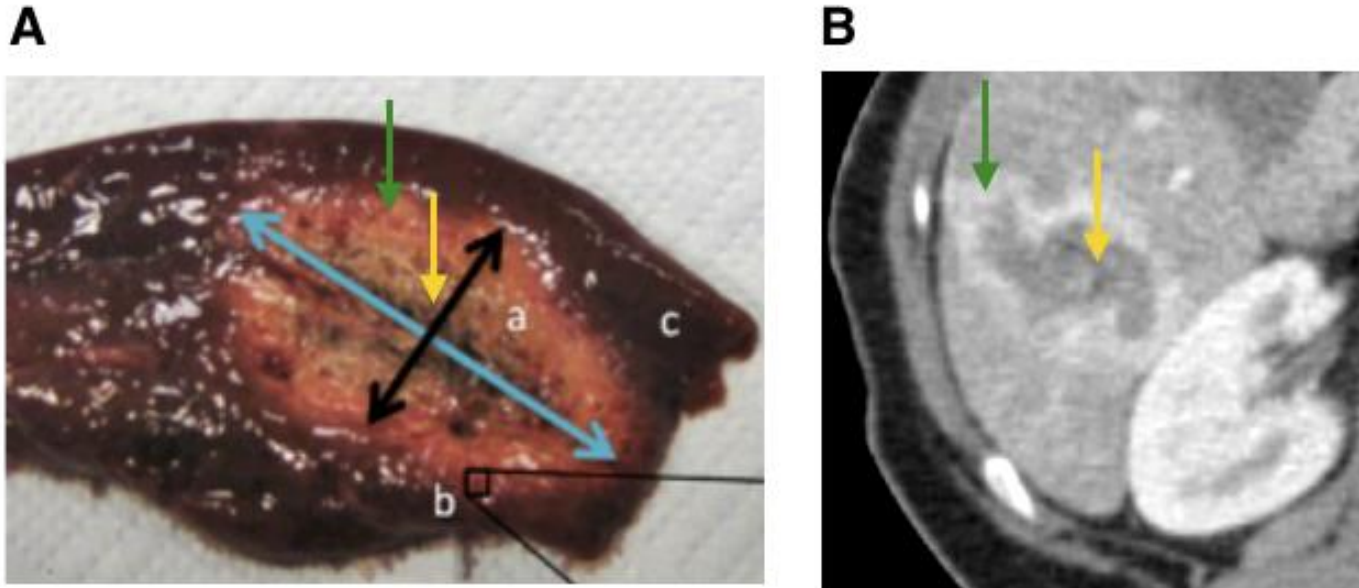


Context: Microwave liver ablation

- Treated region (ablation zone):
 - Inner “white zone”: complete cell death
 - Outer “red zone”: incomplete cell death, hyperaemia, and inflammation
 - Immunologically active and pro-oncogenic.
- To assess for treatment efficacy: a contrast enhanced CT scan is performed at the end of the procedure.
- New and unique circumstance for which scanning protocols have not been optimised or standardised yet.



Context: Microwave liver ablation



Siriwardana PNP et al, 2015.

Pathological and CT correlates of a microwave ablation zone.

Green arrows: red zone

Yellow arrows: white zone

A: gross pathology of harvested pig liver demonstrating a microwave ablation zone.

B: Post contrast venous phase CT image following microwave liver ablation.



Materials and methods



Study participants

Retrospective matched
legacy control cohort



Single venous phase CT of
the whole liver
Prior to optimisation
n = 20

Prospective
optimisation cohort



Dynamic contrast
enhanced monitoring
scans
Venous phase CT imaging
n = 37

Optimised cohort



Optimised biphasic (late
arterial and venous) CT
imaging
n = 20



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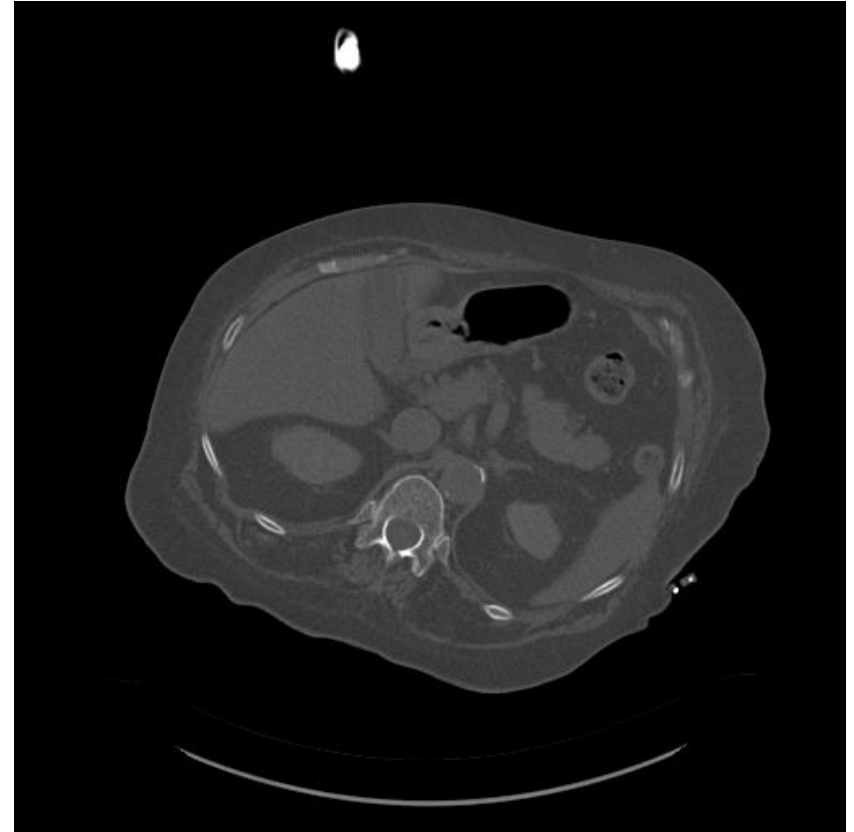


Optimised biphasic (late
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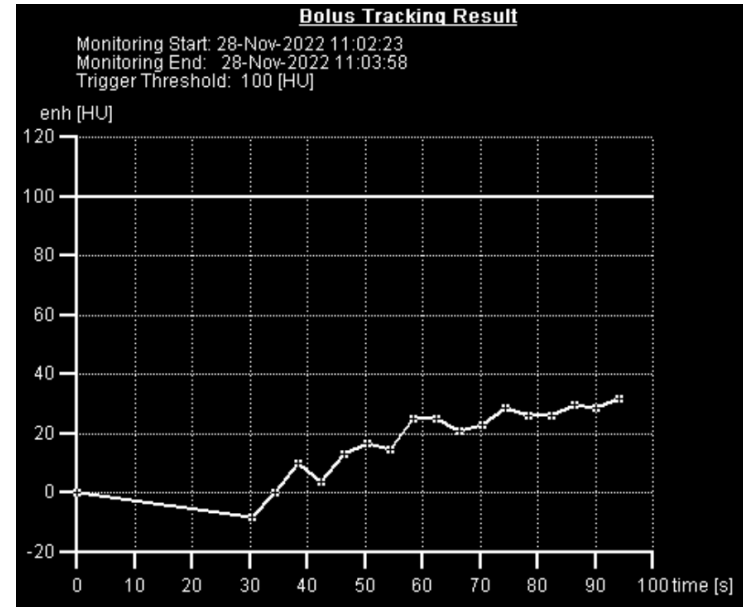


Study participants – Optimisation cohort

- Main goal: determine optimal contrast resolution/scan timings;
- Single unenhanced pre-monitoring slice;
- Twenty sequential low dose, single 10 mm axial slice monitoring scans
 - 120 kV, 40 mA, 0.5 second rotation time, 10 mm collimation.



Study participants – Optimisation cohort



- Enhancement time series through ablation zones (monitoring)
- Pre-contrast slice (pre-monitoring slice)
- Radiation dose increase: about 0.4 mSv (0.02 mSv per monitoring slice)
 - Less than the measured variability in radiation dose (about 1 mSv) resulting from operator choices such as the scan range.
- Helical scan of the whole liver acquired at the end of the dynamic study.



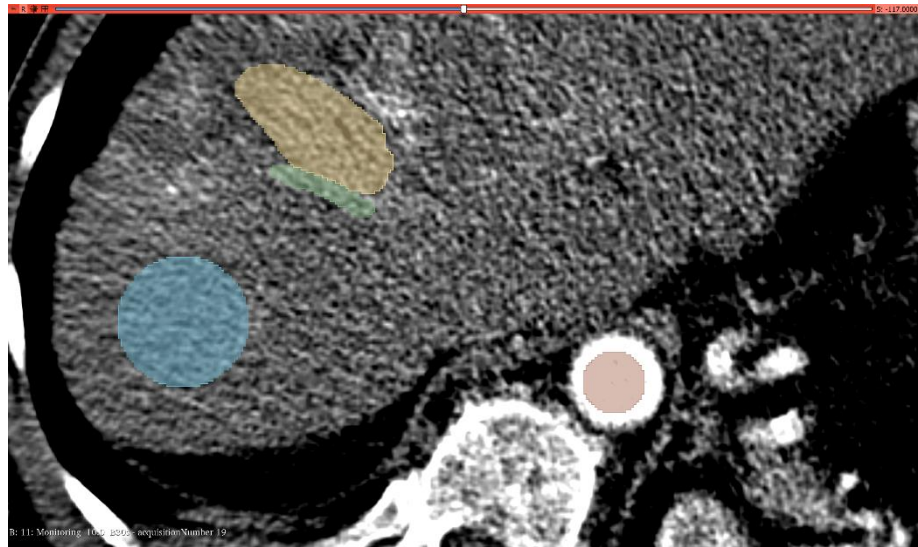
Ablation procedures

- Patients under general anaesthesia;
- High frequency jet ventilation to minimize respiratory excursion;
- CT scanner: Siemens Definition Edge;
- Two microwave generators were used: NeuWave, Johnson & Johnson, WI; Solero, Angiodynamics, NY;
- Antennae were positioned using either freehand or robotic guidance (MAXIO, Perfint PVT, Chennai, In);
- Different numbers of antennae, overlapping ablation zones, and time/power combinations according to operator discretion.



Quantitative image analysis of optimisation cohort and selection of optimised protocol

- Monitoring slices that visually had the greatest contrast between red zone, white zone, and parenchyma were selected for segmentation using 3D Slicer



Quantitative image analysis of optimisation cohort and selection of optimised protocol

- ROIs were labelled, exported as DICTOM RT structure set objects, and analysed using Python:
 - HU values for each ROI along the whole dynamic time series were extracted:
 - Median and interquartile range of each ROI histogram were plotted versus time;
 - Contrast-to-noise ratio (CNR) between red zone and parenchyma and white zone and parenchyma
 - Pre-monitoring slice: establish if aorta enhancement could be used to trigger helical scan




Qualitative image analysis in legacy control and optimised cohorts

- Post ablation DICOM images from optimised and legacy cohorts
 - Images were anonymised and transferred to a PACS workstation for visual assessment of IQ;
 - Random order;
 - Assessed independently by two attending radiologists;
 - Unaware of the study purpose and blinded to all clinical information.

1. Very poor quality: cannot see the ablation zone. Non diagnostic.

2. Poor quality/visualization of ablation zone. Somewhat helpful.

 3. Satisfactory quality/visualization of ablation zone. Helpful.

4. Good quality/visualization of ablation zone. Very clear.

5. Excellent quality/ visualization of ablation zone. Exemplary.

Results



Life demands excellence

Study participants

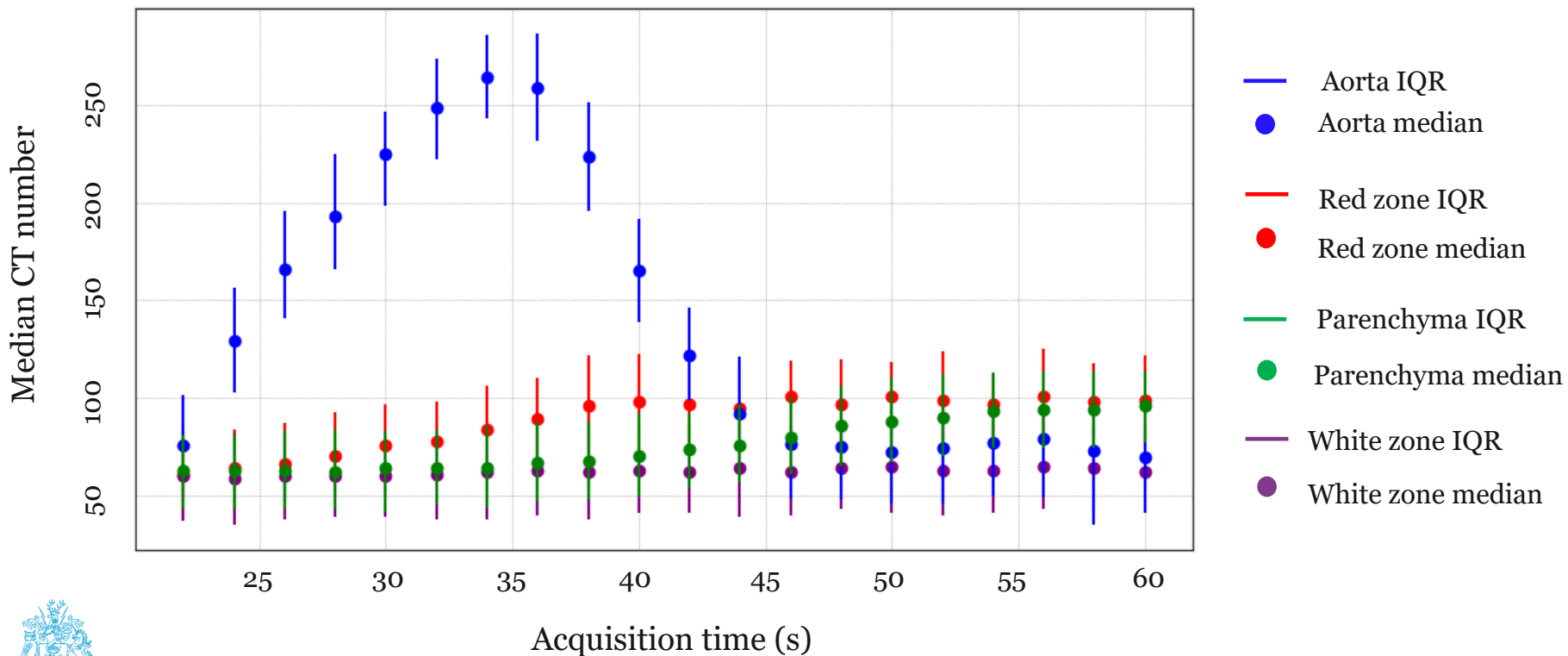
- Seventy-seven participants across three cohorts;
- Median age: 63 years (IQR 50 – 71 years);
- 58% men;
- 140 target liver tumours;
- 78% colorectal cancer metastases;
- 87% performed with robotic guidance;



Analysis of dynamic contrast enhancement curves

Typical enhancement curve

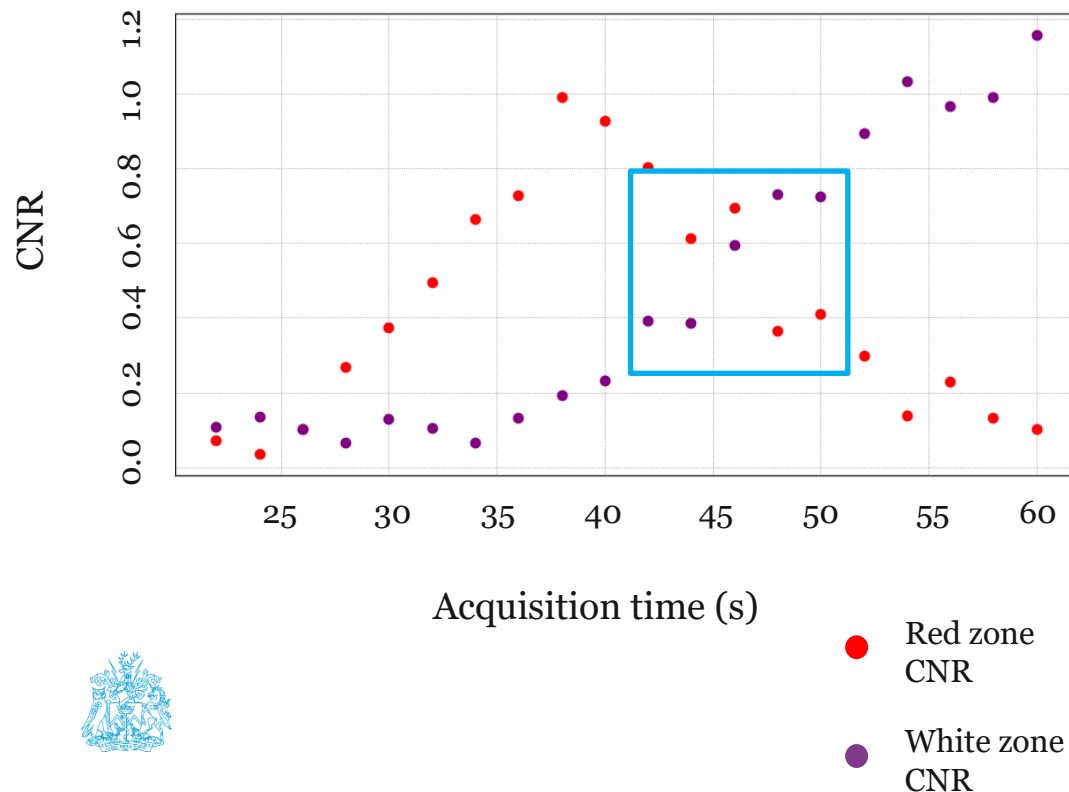
Median CT number vs monitoring slice acquisition time



Analysis of CNR

CNR between red zone and parenchyma and white zone and parenchyma

CNR red zone/parenchyma and CNR white zone/parenchyma



- Start and end time after contrast injection for both CNR values being above 0.4 was highly variable;
- Fixed delay protocol was not considered further.



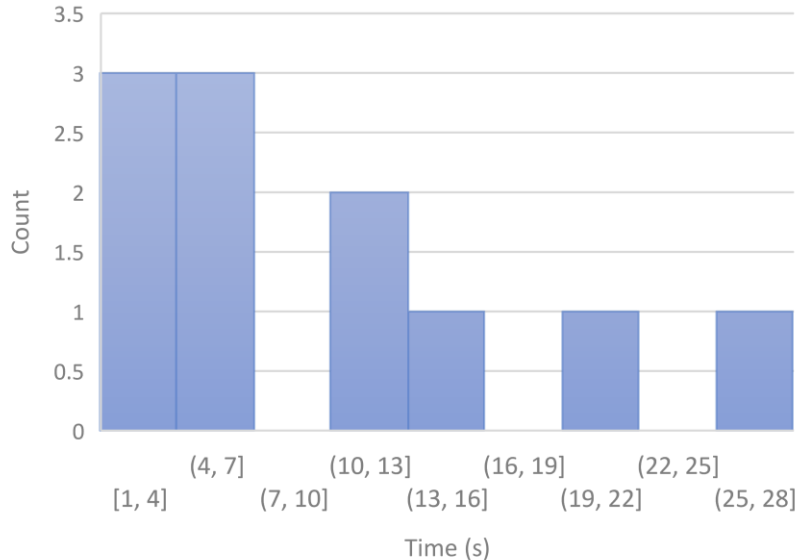
Analysis of CNR

- Bolus tracking technique: use abdominal aorta enhancement as trigger;
- Most studies: peak aorta was at least 200 HU;
- “Adequate contrast window”:
 - Start: difference between time of peak aorta and **minimum** time where both CNRs > 0.4 ;
 - End: difference between time of peak aorta and **maximum** time where both CNRs > 0.4 .

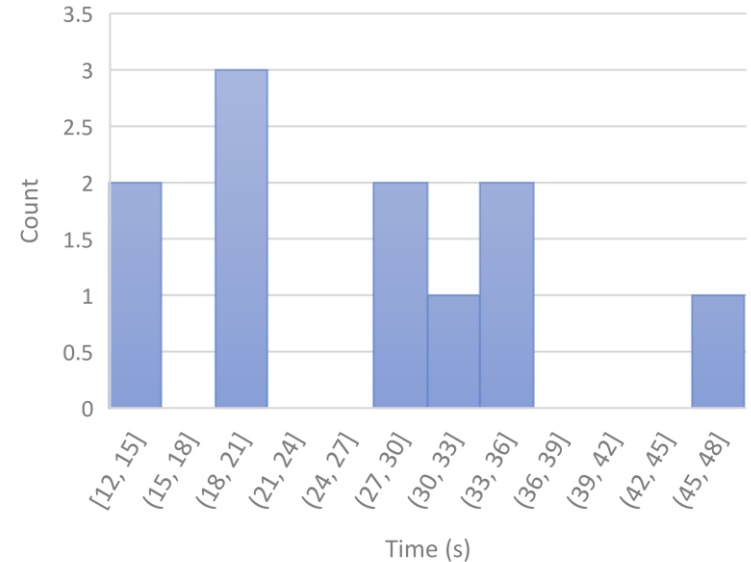


Analysis of CNR

Time (in seconds) between aorta enhancement and start of adequate contrast window



Time (in seconds) between aorta enhancement and end of adequate contrast window



- High variability:
- Some patients presented adequate contrast 1-4 seconds after peak aorta enhancement;
- Others had adequate contrast 26 seconds after the aorta had peaked.



Optimised protocol

- Based on what was observed for most patients:
 - Monitoring scan starting at 20 seconds post contrast initiation.
 - Arterial phase: delay of 12 seconds from 200 HU enhancement in the aorta or from peak aorta if 200 HU wasn't reached;
 - Venous phase: maximum discrimination between white zone and parenchyma (delay of 29 seconds).



Optimised protocol

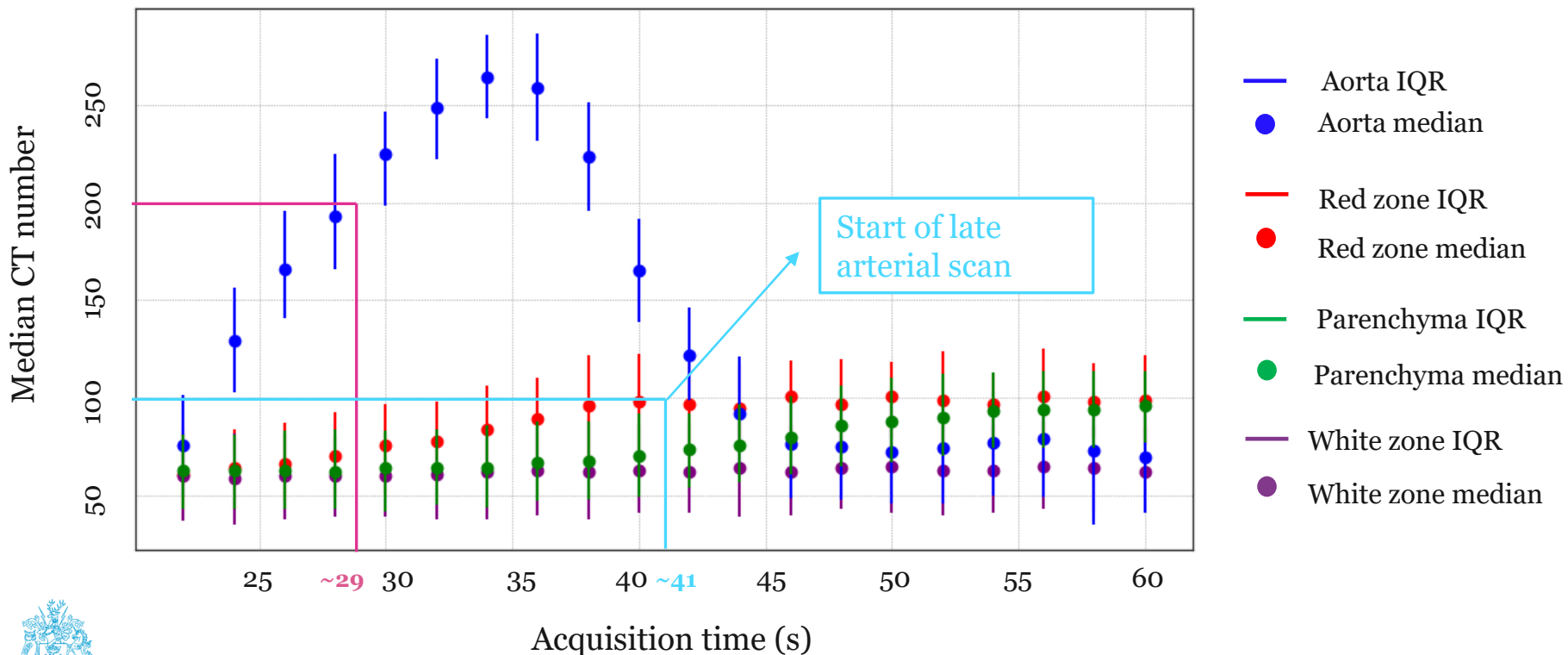
Current protocol used for the liver microwave ablation of patients in the optimised cohort

Parameter	Probe placement phase	Late arterial phase	Portal venous phase
Mode	i-Spiral	Spiral	Spiral
kV	120	120	120
Qref mAs[†]	170	170	170
Rotation time	0.5 s	0.5 s	0.5 s
Pitch	0.8	0.6	0.6
Detector configuration	32 x 1.2 mm	128 x 0.6 mm	128 x 0.6 mm
Delay	n/a	12 seconds from peak aorta	29 seconds from peak aorta
Reconstruction kernel	B3of	B2of and I3of I3of for the robot software	B2of and I3of
Slice thickness	3 mm	3 mm 3 mm	3 mm
Slice interval	3 mm	1 mm for the robot software	3 mm
Contrast volume	n/a	100 ml Omni 350, 5 ml/s	n/a

Analysis of dynamic contrast enhancement curves

Typical enhancement curve

Median CT number vs monitoring slice acquisition time



Qualitative image analysis in legacy control and optimised cohorts

Median visual IQ Likert score (mean of both readers)

Optimised arterial phase studies vs **legacy** control cohort



4.75 vs 2.75 for most recently ablated tumours, $P < 0.0001$

4.75 vs 2.75 for all tumours, $P < 0.001$

Optimised venous phase studies vs **legacy** control cohort



4.25 vs 2.75 for most recently ablated tumours, $P < 0.001$

4.00 vs 2.75 for all tumours, $P < 0.0001$



Conclusions, limitations, and next steps



Summary: conclusions, limitations, and next steps

Conclusions

- New protocol can assist radiologists in judging the efficacy of ablation procedures;
- Decisions regarding repeat ablation can be made with patient still on the table whilst under anaesthesia
 - Increase quality of ablations;
 - Reduce local recurrence;
 - Ultimately: improve survival.



Summary: conclusions, limitations, and next steps

Limitations

- High anatomic variability;
- Wrong timing for monitoring scans: missed peak aorta enhancement;
- Motion artefact;
- Needle artefact;
- No red zone visible.

Next steps

- Image segmentation: comparison between pre-ablation and post-ablation scans
- Assess the impact of the optimised protocol on survival



References

- [1] Xu, Xiao-Lin, et al. "Radiofrequency ablation versus hepatic resection for small hepatocellular carcinoma: systematic review of randomized controlled trials with meta-analysis and trial sequential analysis." *Radiology* 287.2 (2018): 461-472.
- [2] Ruers, Theo, et al. "Local treatment of unresectable colorectal liver metastases: results of a randomized phase II trial." *JNCI: Journal of the National Cancer Institute* 109.9 (2017): djx015.
- [3] Gurusamy, Kurinchi, et al. "Liver resection surgery versus thermal ablation for colorectal LiVer MetAstases (LAVA): study protocol for a randomised controlled trial." *Trials* 19.1 (2018): 1-13.
- [4] Kron, Philipp, et al. "Ablation or resection for colorectal liver metastases? A systematic review of the literature." *Frontiers in oncology* 9 (2019): 1052
- [5] Siriwardana PNPN, Singh S, Johnston EW, et al. Effect of Hepatic Perfusion on Microwave Ablation Zones in an Ex Vivo Porcine Liver Model. *J Vasc Interv Radiol* [Internet] Elsevier; 2015;28(2):1–8. Available from: <http://dx.doi.org/10.1016/j.jvir.2016.03.006>
- [6] Kumar G, Goldberg SN, Gourevitch S, et al. Targeting STAT3 to suppress systemic pro-oncogenic effects from hepatic radiofrequency ablation. *Radiology* 2018;286(2):524–536.
- [7] Chan R, Kumar G, Abdullah B, et al. Optimising the scan delay for arterial phase imaging of the liver using the bolus tracking technique. *Biomed Imaging Interv J* 2011;7(2):e12
- [8] Fedorov A., Beichel R., Kalpathy-Cramer J., Finet J., Fillion-Robin J-C., Pujol S., Bauer C., Jennings D., Fennessy F.M., Sonka M., Buatti J., Aylward S.R., Miller J.V., Pieper S., Kikinis R. 3D Slicer as an Image Computing Platform for the Quantitative Imaging Network. *Magnetic Resonance Imaging*. 2012 Nov;30(9):1323-41. PMID: 22770690. PMCID: PMC3466397.



Acknowledgements

- DR Physics group - The Royal Marsden Hospital, London
- Jodie Basso
- Ed W Johnston



Thank you!



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