

# Evaluation and optimisation of low dose neck CT for SPECT

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## **Context and Background**

Who are we? What do we do? What was the problem?





## Context & background: Who are we?



#### **DR Physics Team at the RMH**

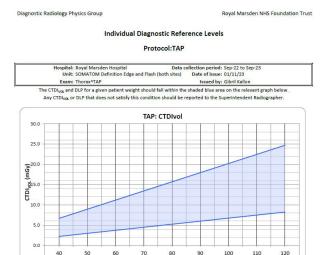
- o 6.2 clinical scientists:
  - o Three MPEs
  - o Two trainee MPEs
  - One vacancy
  - One RT/DR clinical scientist (0.2 WTE)
- o Two trainee clinical scientists
- o 19 CT scanners across 6 sites
  - Including PET/SPECT-CT
- Specialisms across all sites:
  - Oncology
  - Heart and lung (Royal Brompton Hospital)

## Context & background: dose surveys



IR(ME)R 2017 Reg. 13<sup>[1]</sup>: <u>Estimates</u> of population doses

The employer must collect **dose** estimates from medical exposures for radiodiagnostic and interventional procedures, taking into consideration the distribution by age and gender of the exposed population. **Routine dose surveys** for various procedures are conducted in our department approximately every three years to **review and update** LDRLs as needed.



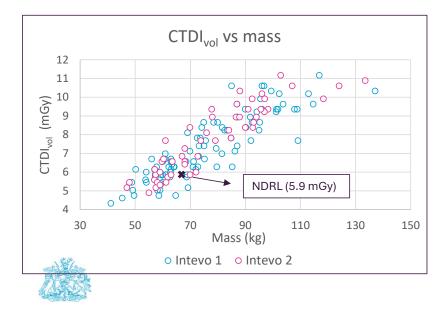
Patient weight (kg)

	proposed local DRLs		
exam	CTDI <sub>vol</sub> (mGy)	DLP (mGycm)	
brain	50	1600	
NTAP	6, 7	620	
TAP	8	547	
TA	6	320	
Т	6	220	
AP	8	420	
CTPA (100 kV)	5	160	
CTPA (120 kV)	7	210	
DIEP	9	360	
Urogram (KUB & 15 min AP)	7,4	470	

## Context & background: the problem

Recent dose survey for low-dose neck CT procedures for SPECT exceeding the NDRLs:

- About 30% for CTDI<sub>vol</sub>,
- > About 50% for DLP.



Dose indicator	Intevo 1	Intevo 2	NDRL <sup>[2]</sup>
CTDI <sub>vol</sub> (mGy):	7.4±1.8	7.7±1.9	5.9
DLP (mGy.cm):	300±75	320±80	210



- Meeting with NM physics and consultants:
  - No justifiable reason
  - > Multidisciplinary optimisation task group put in place.

# What did we do: the journey to the right protocol





## What did we do?

Dosimetry and Imaging Performance Report (16-slice configuration)

#### CARE Dose4D

CARE Dose4D automatically adapts the tube current to the patient's body size and shape.

Using the patient's topogram, CARE Dose4D evaluates two profiles of the patient's X-ray attenuation in the a.p. and lateral directions.

Base on these profiles, the mAs value is adapted to the patient during the subsequent CT scans. The adaption follows an adaptation curve, which determines the correlation between X-ray attenuation and tube current. The adaptation curve has been derived from the clinical optimization for constant diagnostic image quality.

The adaptation curve is based on following three parameters:

- A reference X-ray attenuation, related to a typical adult patient size of approximately 70-80 kg (for adult protocols) respectively a pediatric body size of a 5 year old child with approximately 20kg (for pediatric protocols), which is internally stored in the CT system for the considered organ characteristic and depending on the selected protocol.
  - Brochures;





#### Datasheets;



• System Owner Manual;

The curve below shows the theoretical adaptation curve for a cylindrical body shape. Depending on the individual patient geometry, the curve may deviate from this theoretical function. Moreover, the curve may be cut depending on the system's power limits.

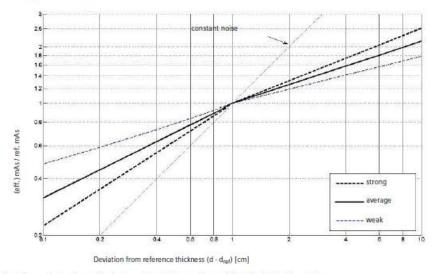
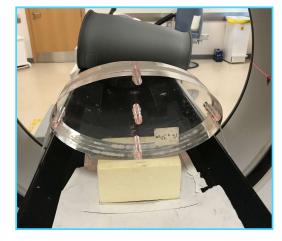


Fig. 6: Adaption of mAs to patient attenuation with adjustable strengths

## What did we do?

- SPECT-CT scanners:
  - o Siemens Symbia Intevo
  - o Siemens Symbia Intevo Bold
- o Assessment of tube current modulation
  - Patients
  - Phantom
- o Phantom work
  - Topogram direction
  - Organ characteristic
  - ≻ kV
  - Pitch
  - Rotation time
  - > Quality reference mAs.





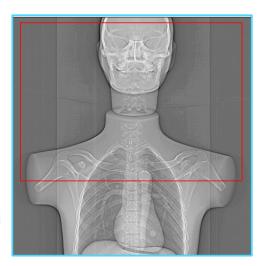




## **Protocol changes**

#### Parameters of existing protocol:

- Topogram direction: AP
- o 130 kV
- o Quality reference mAs: 35
- Organ characteristic: Neck
- o Pitch: 0.8
- o Rotation time: 1 second



#### Parameters to test:

Organ characteristic: Neck, shoulders, chest, abdomen

**kV:** 130, 110

Topogram direction: AP, LAT

**Pitch:** 0.8, 1.1, 1.2, 1.5

Rotation time: 0.6 s, 1 s

Quality reference mAs: 28, 35

Lots of possible combinations, not all of them good/worth trying!



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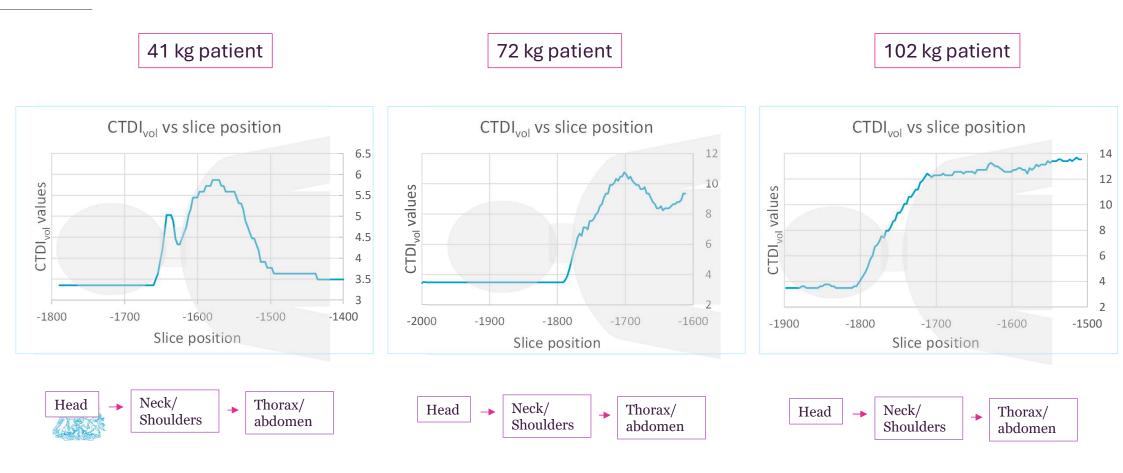
## Results

# What we learned (and what we did about it)





## Results: mAs analysis vs slice position



## Results: mAs analysis vs slice position: phantom

Tube current reaching **minimum** value:

- No modulation regardless of OC used.
- Chest and Shoulders OC examples below:
  - > NB: other parameters (kV, Q<sub>ref</sub> mAs, pitch) unchanged in these charts.



## What we learned so far

#### **Feedback from Siemens:**

- It makes no difference if you use a LAT or AP topogram;
- The lateral topogram is preferred if scanning the spine as you can see the vertebrae better;
- Shoulders are extremely dense in the lateral projections;



*"It's one of those CT protocols that doesn't really fit a standard CT protocol."* 

In the CT world they would most likely scan the neck and chest separately, but this sits somewhere between the two and as you know the organ characteristic influences the dose curves."



#### Initial results from experiments:

- Minimum mAs delivered by the scanner: 32
- o Q<sub>ref</sub> mAs: 35
- **Option 1:** keep 130 kV, change OC to chest
  - 16% dose reduction ✓
  - $\circ$  No modulation along the head imes
- **Option 2:** change kV to 110, keep neck as OC
  - 30% dose reduction ✓
  - Change in contrast
  - Still no modulation ×
  - Potential issue for large patients ?
- **Option 3:** more tests at 130 kV, varying other parameters (OC, pitch, rotation time).

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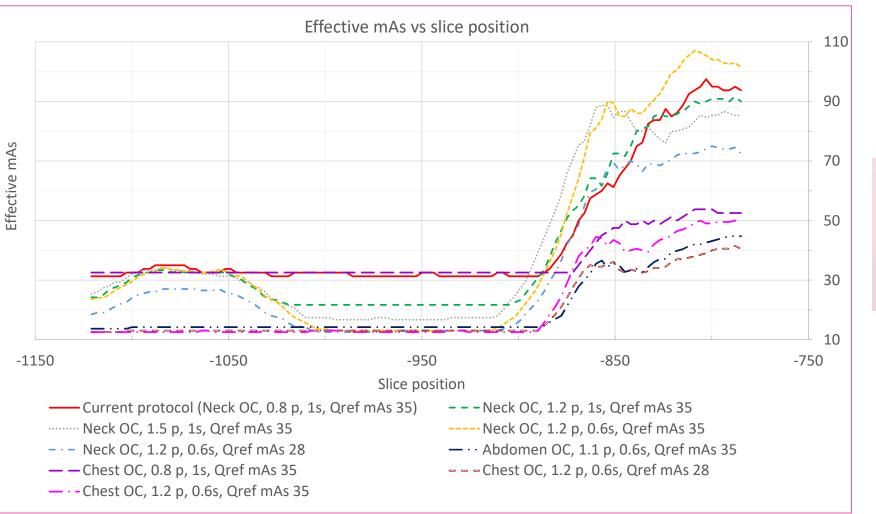
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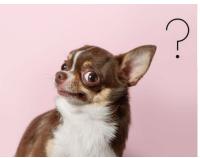
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72

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## Results: 130 kV protocol

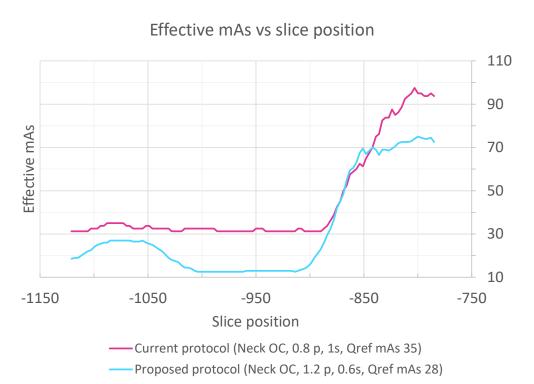




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## Results: 130 kV protocol

Organ characteristic	Pitch	Rotation time (s)	Q <sub>ref</sub> mAs	Post-scan eff mAs	Post-scan CTDI <sub>vol</sub>
Neck	0.8	1	35	48	4.96
Neck	1.2	1	35	45	4.60
Neck	1.5	1	35	44	4.49
Neck	1.2	0.6	35	44	4.55
Neck	1.2	0.6	28	35	3.58
Abdomen	1.1	0.6	35	22	2.34
Chest	0.8	1	35	41	4.20
Chest	1.2	0.6	28	21	2.20
Chest	1.2	0.6	35	24	2.45





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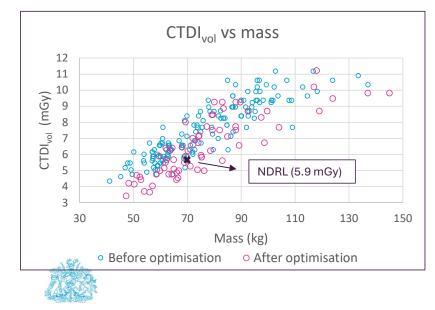
## Where are we at now?





### Where are we at now?

- Data collection period after optimisation:
  20/04/2023 19/02/2024
- o Compared to NDRLs, differences are:
  - About 5% for CTDI<sub>vol</sub>,
  - About 20% for DLP.



Dose indicator	Intevo 1	Intevo 2	NDRL
CTDI <sub>vol</sub> (mGy):	6.2±2.2	6.2±1.9	5.9
DLP (mGy.cm):	260±100	250±80	210

#### <u>RMH scanning length:</u>

- Minimum: 235 mm
- o Median: 430 mm
- o Maximum: 450 mm

<u>N[</u>	ORL scanning length:
0	Minimum: 180 mm
0	Median: 350 mm
$\circ$	Maximum: 430 mm



19 The Royal Marsden

# Conclusions and lessons learned





## **Conclusions and lessons learned**

#### **Conclusion:**

After about one year, we **successfully** reduced the representative dose indicators to **align** with the published **NDRLs**.

Image quality was still deemed acceptable and adequate for the required clinical task.

#### Lessons learned:

- These neck CT scans often extended beyond the neck;
- Not solely used for localisation and attenuation correction:
  - Radiologists still required diagnostic image quality for the lung portion of the scan.

#### More lessons:

- Better understanding of scanner and protocols;
- Joint effort required (NM physicists, technologists, clinicians, apps specialists)
  - E.g., change in rotation time and pitch inevitably led to faster scans
  - Fast scans are good for DR, but was it ok with NM?

#### And a bit more:

- Various protocol options available
  - Professional judgement to choose one.
- Strengthening collaboration across different modalities
- Optimisation: **ongoing process** 
  - Further changes to be discussed.

## References

- 1. The Ionising Radiation (Medical Exposure) Regulations 2017. UK Legislation, 2017.
- 2. Iball, G.R. et al. A national survey of computed tomography doses in hybrid PET-CT and SPECT-CT examinations in the UK. Nuclear Medicine Communications. 2017;38(6):459 to 470
- 3. Siemens Symbia Intevo Data Sheet. (Siemens)
- 4. Siemens Symbia Intevo System Owner's Manual. (Siemens)
- 5. Kyoto Kagaku, C. O. (2020). LTD. Whole body phantom "PBU-60."



## Acknowledgements

- Diagnostic Radiology Physics group The Royal Marsden NHS Foundation Trust
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# Thank you!

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23